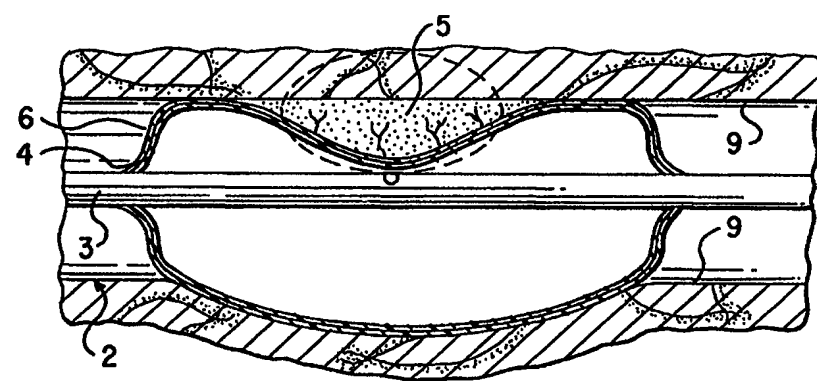


INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(51) International Patent Classification ⁷ : A61L 29/16, 27/54, 31/16, 29/08, 31/10	A1	(11) International Publication Number: WO 00/21584 (43) International Publication Date: 20 April 2000 (20.04.00)
(21) International Application Number: PCT/US99/23654 (22) International Filing Date: 14 October 1999 (14.10.99) (30) Priority Data: 09/172,026 14 October 1998 (14.10.98) US (71) Applicant: SCIMED LIFE SYSTEMS, INC. [US/US]; One Scimed Place, Maple Grove, MN 55311-1566 (US). (72) Inventors: BARRY, James, J.; 35 Jackson Circle, Marlboro, MA 01752 (US). PALASIS, Maria; 65 Martin Road, Wellesley, MA 02181 (US). (74) Agents: CAVANAUGH, David, L. et al.; Kenyon & Kenyon, Suite 700, 1500 K Street, N.W., Washington, DC 20005 (US).		(81) Designated States: AL, AM, AT, AU, AZ, BA, BB, BG, BR, BY, CA, CH, CN, CR, CU, CZ, DE, DK, DM, EE, ES, FI, GB, GD, GE, GH, GM, HR, HU, ID, IL, IN, IS, JP, KE, KG, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MA, MD, MG, MK, MN, MW, MX, NO, NZ, PL, PT, RO, RU, SD, SE, SG, SI, SK, SL, TJ, TM, TR, TT, TZ, UA, UG, UZ, VN, YU, ZW, ARIPO patent (GH, GM, KE, LS, MW, SD, SL, SZ, TZ, UG, ZW), Eurasian patent (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European patent (AT, BE, CH, CY, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE), OAPI patent (BF, BJ, CF, CG, CI, CM, GA, GN, GW, ML, MR, NE, SN, TD, TG). Published <i>With international search report. Before the expiration of the time limit for amending the claims and to be republished in the event of the receipt of amendments.</i>
(54) Title: LOADING AND RELEASE OF WATER-INSOLUBLE DRUGS		
		
(57) Abstract <p>A medical device, polymer composition, and method for delivering substantially water-insoluble drugs to tissue at desired locations within the body. At least a portion of the exterior surface of the medical device is provided with a polymer coating. Incorporated in the polymer coating is a solution of at least one substantially water-insoluble drug in a volatile organic solvent. The medical device is positioned to a desired target location within the body, whereupon the drug diffuses out of the polymer coating.</p>		

FOR THE PURPOSES OF INFORMATION ONLY

Codes used to identify States party to the PCT on the front pages of pamphlets publishing international applications under the PCT.

AL	Albania	ES	Spain	LS	Lesotho	SI	Slovenia
AM	Armenia	FI	Finland	LT	Lithuania	SK	Slovakia
AT	Austria	FR	France	LU	Luxembourg	SN	Senegal
AU	Australia	GA	Gabon	LV	Latvia	SZ	Swaziland
AZ	Azerbaijan	GB	United Kingdom	MC	Monaco	TD	Chad
BA	Bosnia and Herzegovina	GE	Georgia	MD	Republic of Moldova	TG	Togo
BB	Barbados	GH	Ghana	MG	Madagascar	TJ	Tajikistan
BE	Belgium	GN	Guinea	MK	The former Yugoslav Republic of Macedonia	TM	Turkmenistan
BF	Burkina Faso	GR	Greece	ML	Mali	TR	Turkey
BG	Bulgaria	HU	Hungary	MN	Mongolia	TT	Trinidad and Tobago
BJ	Benin	IE	Ireland	MR	Mauritania	UA	Ukraine
BR	Brazil	IL	Israel	MW	Malawi	UG	Uganda
BY	Belarus	IS	Iceland	MX	Mexico	US	United States of America
CA	Canada	IT	Italy	NE	Niger	UZ	Uzbekistan
CF	Central African Republic	JP	Japan	NL	Netherlands	VN	Viet Nam
CG	Congo	KE	Kenya	NO	Norway	YU	Yugoslavia
CH	Switzerland	KG	Kyrgyzstan	NZ	New Zealand	ZW	Zimbabwe
CI	Côte d'Ivoire	KP	Democratic People's Republic of Korea	PL	Poland		
CM	Cameroon	KR	Republic of Korea	PT	Portugal		
CN	China	KZ	Kazakstan	RO	Romania		
CU	Cuba	LC	Saint Lucia	RU	Russian Federation		
CZ	Czech Republic	LI	Liechtenstein	SD	Sudan		
DE	Germany	LK	Sri Lanka	SE	Sweden		
DK	Denmark	LR	Liberia	SG	Singapore		
EE	Estonia						

LOADING AND RELEASE OF WATER-INSOLUBLE DRUGS

This application is a continuation-in-part of co-pending application serial no. 09/133,603, filed August 13, 1998, which is a continuation-in-part of co-pending application serial no. 08/910,136, filed August 13, 1997, both of which are incorporated herein in their entirety by reference thereto.

10 FIELD OF THE INVENTION

The invention relates to methods and devices for the localized delivery of substantially water-insoluble drug agents within the body.

15 BACKGROUND

The systemic administration of drug agents, such as by transoral or intravenous means, treats the body as a

whole even though the disease to be treated may be localized. In such a case, systemic administration may not be desirable because, for example, the drug agents may have unwanted effects on parts of the body which are not to be treated, or because treatment of the diseased part of the body requires a high concentration of drug agent that may not be achievable by systemic administration.

It is therefore often desirable to administer drug agents at a localized site within the body. Common examples include cases of localized disease or occluded body lumens. Various methods have been proposed for such localized drug administration. For example, U.S. Patent No. 5,304,121, hereby incorporated by reference, discloses a method of delivering water-soluble drugs to tissue at desired locations of a body lumen wall. The method generally includes the steps of impregnating a hydrogel polymer on an expandable catheter with an aqueous drug solution, inserting the catheter into a blood vessel to a desired location, and expanding the catheter against the surrounding tissue allowing the release of the drug to the tissue. This method of localized drug delivery using hydrogel polymer impregnation has a limitation of being applicable to drug agents which are dissolved in water at

concentrations sufficient for therapeutic gel loading levels. There thus exists a need for a method and apparatus for the localized delivery of drug agents within the body, where the drug agents are substantially water-insoluble. Moreover, there exists a need for a method and implantable device that provides a sustained release of such substantially water-insoluble drug agents over a time frame effective to inhibit proliferative disease.

SUMMARY OF THE INVENTION

One objective of the present invention is to provide a method and apparatus for the localized delivery of substantially water-insoluble drug agents to predetermined locations within the human body.

A further objective of the present invention is to provide a method and apparatus to facilitate gradual, localized release of drug agents at predetermined locations within the human body.

A further objective of the invention is to administer drug agents by diffusion directly into the tissue requiring treatment. The drug is preferably applied in a manner that does not further injure the tissue to be treated, and administration is selectively and evenly distributed over the treated area such that the drug can be

taken up by the tissue, without, for example, being washed away by body fluids.

The present invention provides methods and medical devices for the localized delivery of substantially water-insoluble drugs agents.

A particular embodiment of the present invention features a catheter and method for delivering substantially water-insoluble drug agents to tissue at a desired location along body lumen walls. The catheter is constructed for insertion in a body lumen and has a catheter shaft and an expandable portion mounted on the catheter shaft. The expandable portion is expandable to fill the cross-section of the body lumen. At least a portion of the exterior surface of the expandable portion is defined by a polymer coating. Incorporated into the polymer coating is at least one substantially water-insoluble drug. The catheter is positioned to a desired target location within the body, whereupon the polymer coating absorbs water, thus dissolving the drug and resulting in the diffusion of the drug out of the polymer coating. The polymer and drug are selected to allow controlled release of a desired dosage of the drug from the polymer.

Another particular embodiment of the present

invention features a stent for the localized delivery of substantially water-insoluble drug agents to tissue at a desired location along body lumen walls. The stent is at least partially coated with a polymer coating having at least one substantially water-insoluble drug therein. The stent configuration, polymer and drug are selected to allow for the controlled release dosage and release rate of the drug from the polymer.

In a most preferred embodiment, the stent is a patterned stent for the localized delivery of paclitaxel to tissue at a desired location along body lumen walls. The stent is at least partially coated with a polymer/paclitaxel matrix that provides sustained release of paclitaxel at the desired site within the lumen wall.

In another aspect of the invention, there is provided a method for preventing or inhibiting proliferative disease in a patient comprising implanting a patterned stent comprising an outer coating of polymer/paclitaxel at a site of cellular proliferation, wherein the paclitaxel is released from the outer coating at a release rate and for a period of time sufficient to inhibit or prevent cellular proliferation at the site.

BRIEF DESCRIPTION OF THE DRAWINGS

Fig. 1a shows one embodiment of the present invention in which a drug solution is impregnated into a polymer-coated balloon catheter.

5 Fig. 1b shows the insertion of a polymer-coated balloon catheter into a body lumen, in accordance with the present invention.

10 Fig. 1c shows the expansion of a polymer-coated balloon catheter at an occlusion site within a body lumen, in accordance with the present invention.

Fig. 2 shows a drug delivery balloon catheter embodiment of the present invention including a sheath for covering the catheter as it is being moved through a vessel toward the occlusion to be treated.

15 Figs. 3a and 3b show the release profile of paclitaxel from a balloon catheter having a polyacrylic acid-based coating for up to 50 and 5000 minutes, respectively, in accordance with the present invention.

20 Figs. 4a and 4b show the release profile of dexamethasone from a balloon catheter having a polyacrylic acid-based coating for up to 30 and 400 minutes, respectively, in accordance with the present invention.

Fig. 5 shows the release profiles of molsidomine

from various balloon catheters having a polyacrylic acid-based coating for up to 5 minutes, in accordance with the present invention.

5 Fig. 6 shows the release profiles of dexamethasone from various balloon catheters having a polyacrylic acid-based coating for up to 450 minutes, in accordance with the present invention.

10 Figs. 7a and 7b show the release profiles of water-soluble and substantially water-insoluble estradiol from balloon catheters having a polyacrylic acid-based coatings for up to 10 and 200 minutes, respectively, in accordance with the present invention.

15 Fig. 8 shows the release profile of paclitaxel for up to 10 days from polyurethane coated stents dipped in 30 mg/ml paclitaxel in ethanol for 3 days, in accordance with the present invention.

Fig. 9 shows the release profiles of paclitaxel from various polyurethane-coated balloon catheters for up to 2 hours, in accordance with the present invention.

20 Fig. 10 shows the cumulative release profile of paclitaxel over a time frame of days. This figure shows the cumulative release of paclitaxel for delivery rates of 5 μ g/day and 0.5 μ g/day.

DETAILED DESCRIPTION

The present invention provides methods and medical devices for the localized delivery of one or more substantially water-insoluble drug agents to predetermined locations within the human body, such as within the vascular system, urinary tract, prostate, esophagus, colon, brain, etc.

In accordance with an embodiment of the invention, a substantially water-insoluble drug agent is dissolved in a volatile organic solvent. "Organic solvent" is intended to mean a singular organic solvent or a solvent mixture having at least one organic component. The solvent mixture also includes mixtures of water with miscible organic solvents. The drug solution is then applied to a polymer coating on a medical device that is adapted for insertion into the body. Examples of such medical devices include catheters, guide wires, balloons, filters (e.g., vena cava filters), stents, stent grafts, vascular grafts, intraluminal paving systems, implants and other devices used in connection with drug-loaded polymer coatings. Such devices are implanted or otherwise utilized in body lumina and organs such as the coronary vasculature, esophagus, trachea, colon, biliary tract, urinary tract, prostate,

brain, and the like. Examples of suitable vascular grafts are described in U.S. Pat. Nos. 5,509,931, 5,527,353, and 5,556,426. Vena cava filters such as those described in WO 96/12448 and WO 96/17634 may also be used
5 in the present invention. All of foregoing documents identified by number are incorporated herein in their entireties.

The filters that can be provided with a polymeric material/drug-agent matrix in accordance with the present
10 invention include, for example, thrombus filters that can be placed at a selected location within the vascular system and removed when no longer required. A preferred location for placement of these filters is the vena cava. Filters placed in the vascular system can intercept blood clots
15 that may otherwise travel to the lungs and result in a pulmonary embolism, a life-threatening emergency that has become increasingly common. In one embodiment of the present invention there is provided such an implanted vascular filter having a polymeric material/drug outer
20 coating thereon. In a most preferred embodiment, the filter has a polymeric material/paclitaxel outer coating, and most preferably, a polylactic acid/polycaprolactone copolymer/paclitaxel coating. The polymeric coating may

also have incorporated therein or thereon any other therapeutic agent that is used for reducing the formation of, or complications due to, clot formation or neointima formation. Such agents, include, but are not limited to
5 antithrombogenic agents and thrombolytic agents and other antiproliferative agents.

Further examples of filters that may be provided with the polymeric material/drug coating in accordance with present invention include, e.g., those described in
10 International Application No. WO 96/17634 and International Application No. WO 96/12448, both of which are herein incorporated by reference.

The grafts, including stent grafts, that can be provided with a polymeric material/drug agent matrix in
15 accordance with the present invention include synthetic vascular grafts that can be used for replacement of blood vessels in part or in whole. A typical vascular graft is a synthetic tube with each end thereof sutured to the remaining ends of a blood vessel from which a diseased or
20 otherwise damaged portion has been removed. In a typical stent graft, each end of the synthetic tube portion includes a stent that is affixed to each of the remaining ends of a blood vessel from which a diseased or otherwise

damaged portion has been removed. Alternatively, in a stent graft, the replacement vessel may be segment of a vessel removed from another location in the patient, such as a portion of a femoral artery or the like. In the case
5 of a synthetic graft, the graft is typically tubular and may be, e.g., of a woven, knit or velour construction. Preferred materials for the grafts and covering material for the stent grafts include polyethylene terephthalate and polytetrafluoroethylene. The vascular grafts may be
10 reinforced with, for example, helices, rings, etc. in order to provide uniform strength over the entire surface of the graft tubing. The materials of which such grafts are constructed are biologically compatible materials including, but not limited to, thermoplastic materials such
15 as polyester, polytetrafluoroethylene (PTFE), silicone and polyurethanes. The preferred materials include polyester fibers and PTFE.

Examples of other suitable grafts are described in U.S. Pat. Nos. 5,509,931, 5,527,353, and 5,556,426, all
20 of which are herein incorporated by reference. In a most preferred embodiment of the invention, the graft is provided with a coating of polymeric material/paclitaxel, and most preferably, the polymeric material is a copolymer

of polycaprolactone and polylactic acid. This paclitaxel-coated graft, when positioned at a desired site in the body provides an extended release of paclitaxel to the site.

5 A polymeric material/drug agent matrix in accordance with the present invention may be used as an intraluminal paving system. In such intraluminal paving systems as are known in the art, the polymeric material/drug agent matrix will typically be applied directly to an interior surface of vascular or non-vascular lumina. An intraluminal paving
10 system is formed, for example, by admixing a drug agent with a liquid polymer, in the absence of a solvent, to form a liquid polymer/drug agent mixture. The mixture is then applied directly to a luminal surface by any conventional method, such as by injecting the mixture against the
15 luminal surface. Curing of the mixture typically occurs in-situ. To facilitate curing, a cross-linking or curing agent may be added to the mixture prior to application thereof to the luminal surface. Addition of the cross-linking or curing agent to the polymer/drug agent liquid
20 mixture must not occur too far in advance of the application of the mixture to the luminal surface in order to avoid over-curing of the mixture prior to application thereof to the luminal surface. Curing may also occur in-

situ by exposing the polymer/drug agent mixture, after application to the luminal surface, to radiation such as ultraviolet radiation or laser light, heat, or by contact with metabolic fluids such as water at the site where the mixture has been applied to the luminal surface. In a preferred intraluminal paving system in accordance with the invention, the drug agent is paclitaxel and the paclitaxel may be incorporated in the polymeric material alone or in combination with another drug agent. In intraluminal paving systems in accordance with a preferred embodiment of the present invention, the polymeric material incorporating the paclitaxel and, if desired, any additional therapeutic agent(s), may be either bioabsorbable or biostable. Any of the polymers described herein that may be formulated as a liquid may be used to form the polymer/drug agent mixture for use as an intraluminal paving system.

In a preferred embodiment, the polymer used to coat the medical device is provided in the form of a coating on an expandable portion of a medical device. After applying the drug solution to the polymer and evaporating the volatile solvent from the polymer, the medical device is inserted into a body lumen where it is positioned to a target location. In the case of a balloon

catheter, the expandable portion of the catheter is subsequently expanded to bring the drug-impregnated polymer coating into contact with the lumen wall. The drug is released from the polymer as it slowly dissolves into the aqueous bodily fluids and diffuses out of the polymer. This enables administration of the drug to be site-specific, limiting the exposure of the rest of the body to the drug.

The polymer used in the present invention is preferably capable of absorbing a substantial amount of drug solution. When applied as a coating on a medical device in accordance with the present invention, the dry polymer is typically on the order of from about 1 to about 50 microns thick. In the case of a balloon catheter, the thickness is preferably about 1 to 10 microns thick, and more preferably about 2 to 5 microns. Very thin polymer coatings, e.g., of about 0.2-0.3 microns and much thicker coatings, e.g., more than 10 microns, are also possible. It is also within the scope of the present invention to apply multiple layers of polymer coating onto a medical device. Such multiple layers are of the same or different polymer materials.

The polymer of the present invention is

hydrophilic or hydrophobic, and is selected from the group consisting of polycarboxylic acids, cellulosic polymers, including cellulose acetate and cellulose nitrate, gelatin, polyvinylpyrrolidone, cross-linked polyvinylpyrrolidone, 5 polyanhydrides including maleic anhydride polymers, polyamides, polyvinyl alcohols, copolymers of vinyl monomers such as EVA, polyvinyl ethers, polyvinyl aromatics, polyethylene oxides, glycosaminoglycans, polysaccharides, polyesters including polyethylene 10 terephthalate, polyacrylamides, polyethers, polyether sulfone, polycarbonate, polyalkylenes including polypropylene, polyethylene and high molecular weight polyethylene, halogenated polyalkylenes including polytetrafluoroethylene, polyurethanes, polyorthoesters, 15 proteins, polypeptides, silicones, siloxane polymers, polylactic acid, polyglycolic acid, polycaprolactone, polyhydroxybutyrate valerate and blends and copolymers thereof as well as other biodegradable, bioabsorbable and biostable polymers and copolymers. Coatings from polymer 20 dispersions such as polyurethane dispersions (BAYHDROL®, etc.) and acrylic latex dispersions are also within the scope of the present invention. The polymer may be a protein polymer, fibrin, collage and derivatives thereof,

polysaccharides such as celluloses, starches, dextrans, alginates and derivatives of these polysaccharides, an extracellular matrix component, hyaluronic acid, or another biologic agent or a suitable mixture of any of these, for example. In one embodiment of the invention, the preferred polymer is polyacrylic acid, available as HYDROPLUS® (Boston Scientific Corporation, Natick, Mass.), and described in U.S. Pat. No. 5,091,205, the disclosure of which is hereby incorporated herein by reference. U.S. Patent No. 5,091,205 describes medical devices coated with one or more polyisocyanates such that the devices become instantly lubricious when exposed to body fluids. In a most preferred embodiment of the invention, the polymer is a copolymer of polylactic acid and polycaprolactone.

By "substantially water-insoluble drug" is meant any therapeutic agent having a greater solubility in organics than in water. More specifically, such drugs have a water solubility of no greater than 1 part drug to 30 parts water, more typically no greater than 1 part drug to 1,000 parts water. Such solubilities are described as "sparingly soluble" to "very slightly soluble" in the art.

The drug agents used in the present invention are selected from a number of drug types depending on the

desired application. For example, these drugs include anti-inflammatory agents such as dexamethasone, prednisolone, corticosterone, budesonide, estrogen, sulfasalazine, mesalamine, and analogues thereof; 5 antineoplastic/ antiproliferative/anti-miotic agents such as paclitaxel, 5-fluorouracil, cisplatin, vinblastine, vincristine, epothilones, endostatin, angiostatin, thymidine kinase inhibitors, and analogues thereof; anesthetic agents such as lidocaine, bupivacaine, 10 ropivacaine, and analogues thereof; anti-coagulants; and growth factors.

The drug agents useful in accordance with the present invention may be used singly or in combination. For example, an anti-proliferative agent such as paclitaxel may 15 be used in combination with another drug agent, such as an anticoagulant, anti-inflammatory, antithrombogenic, thrombolytic, nitric oxide-containing polymer, or a vascular cell promoter such as VEGF, for example.

Paclitaxel is a preferred drug agent for use in 20 accordance with the present invention either alone or in combination with another drug agent, as described above. Paclitaxel is a complex alkaloid extracted from the Pacific Yew *Taxusbrevifolia* Family (Family Taxacea) which has been

demonstrated to have antiproliferative activity. As used herein, paclitaxel includes the alkaloid and any pharmacologically active derivative or analog thereof. Thus paclitaxel includes naturally occurring forms and derivatives thereof and synthetic and semi-synthetic forms thereof. TAXOL® is a commercially available form of paclitaxel.

In accordance with the present invention, the drug agents are dissolved in a volatile organic solvent such as, for example, ethanol, isopropanol, chloroform, acetone, pentane, hexane, or methylene chloride, to produce a drug solution. In the case of paclitaxel the preferred solvent is chloroform. The drug solution is then applied to the polymer. A volatile organic solvent typically is selected to provide drug solubilities much greater than the corresponding aqueous solubility for the substantially water-insoluble drug. Accordingly, application of the drug solution to the polymer often results in drug loadings that are orders of magnitude greater than loadings that can be achieved by application of a saturated aqueous solution of the drug to the polymer.

The drug solution is applied to the polymer coating by any suitable means, including dipping the

polymer coating into the drug solution or by applying the solution onto the coating such as by pipet or by spraying, for example. In the former method, the amount of drug loading is controlled by regulating the time the polymer is immersed in the drug solution, the extent of polymer cross-linking, the concentration of the drug in the solution and/or the amount of polymer coating. In another embodiment of the invention, the drug is incorporated directly into the polymer prior to the application of the polymer topcoat as a coating onto a medical device.

After applying the drug solution to the polymer coating, the volatile solvent is evaporated from the coating, for example, by drying in air or in an oven.

The release profile of the drug from the polymer coating is determined by many factors including the drug solubility, amount of drug applied and the thickness and porosity of the polymer coating.

In a preferred embodiment of the present invention, one or more additional layers may be applied over at least a portion of a medical device previously coated with a polymer/drug agent in accordance with the present invention. Desirably, such an additional layer will be provided to modify or modulate the release of one or more

of the drug agents in the underlying layer. For example, a polymeric coating may be applied over the previously applied polymer/drug agent coating to modulate the release rate of the drug agent in that layer. This additional
5 release rate-modifying or modulating layer may be applied in a subsequent coating step in a manner similar to that disclosed herein, for example by spraying a polymer solution onto the previously applied coating layer or by dipping the previously coated medical device into a
10 solution of the polymer selected to form the modifying or modulating layer. However, other methods for applying polymeric materials to substrates, including, for example, in-situ polymerization methods such as plasma polymerization may also be used to provide the additional
15 release rate-modifying or modulating polymeric layer. Such other application processes included within the scope of the present invention are those that will not detrimentally affect the previously applied layer, including the drug agent(s) incorporated therein or thereon. The additional
20 layer may also include one or more additional drug agents including any of the drug agents incorporated into the underlying polymer/drug agent coating layer. Prior to application of the modifying or modulating layer, any

conventional adhesion promotion agent may be applied to the previously applied coating, or other treatment thereof may be conducted, in order to promote adhesion of the modifying or modulating layer to the previously applied coating.

5 Where the modifying or modulating layer is applied in a manner similar to the underlying layer, the polymeric material used for the modifying or modulating layer can be any of the polymers described herein. Where such polymeric material is applied, for example, by plasma polymerization,

10 the polymers are those that can be formed by monomers in a gas phase that can be activated for example by radio frequency waves. Such monomers include, for example, silicone-based monomers such as cyclic or acyclic siloxanes, silanes, silylimidazoles; fluorine-based monomers such as hydrofluorocarbons; aliphatic or aromatic hydrocarbons; acrylic monomers; and combinations thereof.

15 The monomer gas may have functional groups that facilitate later attachment of drug agents thereto by covalent bonding, for example. Any appropriate polymer for the modifying or modulating layer is preferably selected to have a porosity that provides the modifying or modulating effect as described above. The porosity of this polymeric material may also be modified by addition of porosigens or

20

other porosity-affecting adjuvants that are conventionally added to polymers for this purpose. Other factors guiding the selection of a modulating or modifying polymer include, but are not limited to, the thickness of coating layer, the tortuosity of the polymeric material affecting the path of resistance to drug mobility within the polymeric material, the cross-linking density, drug solubility in the modulating or modifying layer, etc. The thickness of the modifying or modulating layer will preferably be less than 5,000 Å, and more preferably in the range of from about 50-2000 Å. A preferred modifying or modulating polymer in accordance with the present invention is a siloxane polymer formed, for example, by a plasma polymerization process. This siloxane modifying or modulating polymer is preferably applied to a medical device that has a polyurethane/drug agent coating previously applied thereto in accordance with the present invention.

When an expandable member such as a balloon catheter is used to administer the drug, pressure can be used to increase the rate of drug transfer to the tissue. An increase in pressure increases the diameter of the balloon and therefore the diameter of the surrounding tissue, thereby increasing the surface area for drug transfer. The

amount of drug that is delivered per unit time is therefore increased.

When an expandable catheter is chosen as the medical device of the present invention, the expandable portion is preferably a balloon, in which case the drug is placed in the polymer for controlled release of the drug upon expansion of the balloon against a body lumen. The expandable portion optionally includes a stent, mountable in a body lumen by expansion thereof. The catheter also optionally comprises a sheath member which is extendable over the expandable portion to inhibit release of the drug into body fluids during placement of the catheter.

Referring now to Figs. 1a-1c, an embodiment for the localized delivery of substantially water-insoluble drugs to a predetermined location within the body is described. The drug administration method shown in Figs. 1a-1c illustrates the use of the present invention in conjunction with an angioplasty process. Catheter device 1 comprises a body 3 having a balloon 4 attached at its distal end. The balloon 4 on the catheter 3 includes a polymer coating 6. As shown in Fig. 1a, drug solution 8 is impregnated into the polymer coating with the balloon in its substantially deflated state prior to insertion into

the patient. As shown in Fig. 1b, after the volatile solvent is evaporated, the device 1 is inserted into a body lumen 2 having a region to be treated, such as an occlusion due to a deposition of plaque 5 on the lumen wall tissue 9.

5 The device 1 is moved along the vessel to position the balloon 4 at the occlusion site, as shown in Fig. 1c. The lumen may be, for example, a narrow, tortuous opening through which the catheter is passed by torquing or other known techniques. As shown in Fig. 1c, the balloon is
10 inflated to provide close contact between the drug-impregnated polymer coating 6 and the surrounding plaque and tissue. As water from the body penetrates into the polymer coating 6, it begins to dissolve the drug agent, which subsequently diffuses out of the polymer coating 6
15 and into the surrounding plaque and tissue.

During drug administration, a substantial amount of the drug contained in the polymer coating is diffused into the affected area. The inflation pressure needed to expand the balloon catheter and dilate the lumen, if
20 necessary, is typically in the range of about 1 to 20 atm. The balloon is formed of any suitable materials such as vinyl polymers such as polyethylene; polyesters such as polyethylene terephthalate; polyamides such as nylon;

polyolefins and copolymers thereof (e.g., Selar, Pebax, Surlyn, Hytrel, etc.). The balloon is optionally a perfusion balloon, which allows blood to perfuse the catheter to prevent ischemia during delivery. A perfusion
5 balloon is particularly preferred for long arterial delivery times and when the delivery drug is only very slightly soluble in water.

Referring to the embodiment of the invention illustrated in Fig. 2, the balloon portion 4 of catheter 3
10 is optionally covered by a protective sheath 7 while the instrument 1 is inserted into a body lumen 2 and positioned at a treatment region. As the coated balloon 4 is positioned at occluded site 5, the protective sheath 7 is drawn back to expose the balloon 4. In an alternative
15 embodiment, the sheath remains stationary while the catheter moves the coated balloon forward into the occluded region. The sheath 7 protects the coating and inhibits premature release of the drug. Such a sheath might be particularly advantageous when using drugs which are not
20 sufficiently water-insoluble or if even minor delivery to tissue during catheter placement is a problem, e.g. for extremely toxic drugs.

Although Figs. 1 and 2 illustrate the application

of the present invention to an angioplasty process, the present invention is also used to administer drug agents to target locations where there is no occlusive formation.

In other embodiments, the medical device of the present invention is an implantable medical device such as a stent, covered stent, stent graft, intraluminal paving system, wire guide, cannulae, artificial limbs, joints, and other prosthetic devices. Where a stent is used it may either balloon- or self-expandable, and is constructed of any biocompatible material. The grafts and covering materials for the stent grafts are made of any biocompatible material such as, for example, polyurethane, polyesters, silicone, or polytetrafluoroethylene.

Stents are generally configured in one of two configurations: patterned or coil. Coil-type stents include, for example, wire stents in the form of coils, spirals or the like, with or without spines, an example of which is the subject of U.S. Pat. No. 4,886,062 (incorporated herein by reference), another example of which is the GR-II[®] (Cook Inc.) stent. Patterned stents used in accordance with a most preferred embodiment of the invention include all stents other than coil-type stents such as, for example, slotted tube stents, criss-cross

tubular stents, braided stents, hexagonal stents, nets, articulated stents, and the like. Patterned stents are also generally preferred over coil stents because they provide more radial support for surrounding body lumina.

5 Preferred patterned stents for use in the present invention include the NIR™ and RADIUS™ stents (SCIMED Life Systems, Inc.) as described in U.S. Pat. No. 5,733,303 and WO 96/26689 (both of which are incorporated herein by reference); the WALLSTENT® (Schneider Inc.) as described in
10 U.S. Pat. Nos. 4,655,771 and 5,061,275 (both of which are incorporated herein by reference); and the SYMPHONY® stent (Boston Scientific Corp.) as described in U.S. Pat. No. 5,540,712 (incorporated herein by reference). The stents and stent grafts described in U.S. Pat. Nos. 5,766,237,
15 5,681,356, 5,522,881 and 5,776,180 (each of which is incorporated herein by reference) and the polymer stents described in U.S. Pat. No. 5,769,883 (incorporated herein by reference) are also within the scope of the present invention.

20 The implantation of a stent, stent graft, vascular graft or filter in accordance with the present invention can be conducted by any medical procedure conventionally used for such implantation. In the case of a stent, a

polymer/paclitaxel coated stent in accordance with the present invention can be fitted over the inflatable element of a balloon catheter and expanded by the balloon to force the stent into contact with the body lumen at or near a site of injury such as, for example, within an injured blood vessel.

Where the medical device in accordance with the present invention is, e.g., a catheter, stent, graft, filter, etc., or any other device used in the vascular system, any blood vessel including arteries, veins and capillaries may be treated in accordance with the present invention. These blood vessels may be in or near any organ in the human or mammalian body.

In a most preferred embodiment of the invention, a patterned stent having a polymer/paclitaxel coating is used to prevent or inhibit proliferative disease. As used herein, "proliferative disease" means any disease or disorder including cancers, malignancies, benign growths and other conditions that result from hyperactivity or hyperplasia of somatic cells, and includes restenosis and vascular hyperplasia such as neointimal hyperplasia. Such proliferative diseases may occur in vascular and other luminal or non-luminal regions of the body.

The inventors have surprisingly found that extended drug release of paclitaxel from a polymer coating on a patterned stent is obtained and consequently, a significant reduction in neointima formation results. The reduction in neointima formation obtained with patterned stents used in accordance with the present invention is surprisingly superior to that obtained using a coiled stent coated with a polymer/paclitaxel matrix. Fig. 10 shows the release rate of paclitaxel obtained with a stent in accordance with the present invention. In a preferred embodiment, paclitaxel is released from a polymer/paclitaxel coated stent for a time period of at least about 28 days after implantation of stent at the desired location within the body. The patterned stent is coated with an outer coating of polymer/paclitaxel such that the amount of paclitaxel is sufficient to prevent, decrease, eliminate or modify cellular proliferation associated with proliferative disease or disorder. The amount of paclitaxel sufficient to inhibit or prevent proliferative disease will vary according to the size of the patterned stents, but is generally in the range of from about 50 μg to 500 μg per stent.

Procedures for preparing a drug delivery medical

device with a polymer coating are presented in the following non-limiting examples.

Example 1: Release kinetics of paclitaxel from polyacrylic acid-based coating.

A 2 mg/ml solution of paclitaxel is prepared in chloroform. The solution is gently agitated until the paclitaxel is completely dissolved. The solution is applied via pipet to a balloon catheter having a polyacrylic acid-based coating and inflated to 2 atm. A total of 100 μ l of solution, and hence 200 μ g of paclitaxel, is applied to the catheter. The balloon catheter is then dried in air for 30 minutes and in a vacuum oven for 48 hours at 50°C to evaporate the chloroform. The catheter is then immersed in a solution of 1% dimethyl sulfoxide (DMSO) and phosphate buffered saline (PBS) having a pH of 7.4 for in-vitro drug release. The cumulative amount of paclitaxel released from the catheter coating yields the data shown in Figs. 3a and 3b.

Example 2: Release kinetics of dexamethasone from polyacrylic acid-based coating.

Solutions containing 1.5 mg/ml and 200 μ g/ml of dexamethasone in chloroform, are prepared by gently
5 agitating until the dexamethasone is completely dissolved. The solutions are separately applied via dripping to separate balloon catheters having polyacrylic acid-based coatings and inflated to 2 atm. A total of 100 μ l of each solution is applied to each respective catheter,
10 corresponding to dexamethasone loadings of 1.5 mg and 200 μ g, respectively. These results can be contrasted with the inability to apply substantial amounts of dexamethasone to polyacrylic acid-based coatings using aqueous solutions, in which case only about 1 μ g of dexamethasone can be loaded
15 into such coatings. The balloon catheters are then dried in a vacuum oven for 2 hours at 50°C to evaporate the chloroform solvent. The catheters are thereafter immersed in PBS (pH = 7.4) to track the release of dexamethasone over time. The cumulative amount of dexamethasone released
20 from each catheter yields the data shown in Figs. 4a and 4b.

Example 3: Release kinetics of molsidomine from polyacrylic acid-based coating.

Various solutions of molsidomine in volatile solvents are prepared and applied to balloon catheters by the methods indicated in Table I. In the "dip" application technique, each balloon catheter having a polyacrylic acid-based coating is dipped into its respective solution for 10 minutes. In the "pipet" application technique, 200 μ l of solution is pipetted onto its respective coated balloon catheter while slowly turning. All samples are dried in an oven for 30 minutes at 50°C and thereafter immersed in PBS (pH = 7.4) to track the release of molsidomine over time. The cumulative amount of molsidomine released from each catheter yields the data shown in Fig. 5a and 5b.

Table I. Molsidomine solution characterization, and methods of applying molsidomine solution to polymer coated catheters.

Sample	Solvent	Concentration (mg Molsidomine per ml solvent)	Application technique
1	chloroform	150	dip
2	chloroform	30	pipet
3	chloroform	150	pipet
4	ethanol	30	pipet
5	ethanol	30	dip

Example 4: Release kinetics of dexamethasone added to polyacrylic acid-based topcoat formulation.

Rather than forming a solution of dexamethasone in an organic solvent and then applying this solution to polymer-coated balloon catheters as in Example 2, dexamethasone is added directly to the polymer used to coat the balloon catheters. Dexamethasone is weighed out into 0.05 g, 0.1 g, and 0.2 g samples, each of which is each added to 1 ml lots of polymer topcoat solution containing polyacrylic acid, methyl ethyl ketone, dimethyl formamide, and t-butyl alcohol. The dexamethasone samples are mixed with the polymer topcoat solutions until completely dissolved. The dexamethasone-containing polymer topcoat solutions are separately applied via dripping to separate, uncoated balloon catheters inflated to 2 atm. After drying in a vacuum oven for 2 hours at 50°C, the catheters are immersed in PBS (pH = 7.4) to track the release of dexamethasone over time. The cumulative amount of dexamethasone released from each catheter yields the data shown in Fig. 6.

Example 5: Comparative release kinetics for water-soluble and water-insoluble estradiol.

Estradiol is provided in both water-soluble and substantially water-insoluble forms. Water-soluble estradiol is applied to a balloon catheter coated with a polyacrylic acid-based coating by i) preparing a 10 mg/ml solution of water-soluble estradiol in deionized, ultra-filtered water; and ii) placing the balloon catheter, inflated to 2 atm, into 200 μ l of the solution for 20 minutes. Water-insoluble estradiol is applied to a balloon catheter coated with a polyacrylic-acid based coating by i) preparing a 10 mg/ml solution of substantially water-insoluble estradiol in methanol; and ii) dripping 100 μ l of the solution onto the balloon catheter. The catheters are thereafter immersed in PBS (pH = 7.4) to track the release of both water-soluble and water-insoluble estradiol over time. Greater release is observed for the substantially water-insoluble form of estradiol when compared to the water-soluble form. The cumulative amount of estradiol released from each catheter yields the data shown in Figs. 7a and 7b.

Example 6: In-vivo delivery of paclitaxel from polyacrylic acid-based coating.

A 9.8 mg/ml solution of radio-labeled paclitaxel in chloroform is prepared. A total of 50 μ l of the solution is applied via pipet to a balloon catheter having a polyacrylic acid-based coating. The paclitaxel from the coated balloon catheter is then released in-vivo to porcine arteries. After release for a predetermined amount of time, the paclitaxel remaining in the coating is extracted using two sequential ethanol washes. The amount of paclitaxel released in the pig bloodstream, as calculated from the amount of paclitaxel loaded into the coating minus that extracted from the coating after delivery, is shown in Table II.

Table II. Amount of paclitaxel released into pig bloodstream from an impregnated, polyacrylic acid-based coated balloon catheter, as a function of delivery time.

Amount of time in bloodstream	Amount of paclitaxel extracted from balloon after delivery (μ g)	Amount of paclitaxel released in bloodstream (μ g)	% of paclitaxel released in bloodstream
1 minute	182 \pm 1	307	63
5 minutes	160 \pm 30	330	68

Example 7: Delivery of paclitaxel to explanted porcine arteries from polyacrylic acid-based coating.

A 9.8 mg/ml solution of radio-labeled paclitaxel in chloroform is prepared. A total of 50 μ l of the solution is applied via pipet to a balloon catheter having a polyacrylic acid-based coating. The coated balloon catheter is then delivered to an explanted porcine artery for 15 minutes. After delivery, the paclitaxel remaining in the coating is extracted using two sequential ethanol washes. The delivered paclitaxel is extracted from the vessel, also by using two sequential ethanol washes. In addition, the vessel is placed in tissue solvent and counted for paclitaxel. Using these extraction methods, at least 80% of the paclitaxel loaded onto the balloon catheter is recovered, as shown in Table III.

Table III. Paclitaxel recovery from ex vivo delivery to porcine artery.

Amount paclitaxel loaded onto balloon	489 μ g
Amount paclitaxel extracted from the balloon after delivery	360 μ g
Amount paclitaxel extracted from artery	30 μ g
Amount paclitaxel counted from tissue solution	1 μ g
Total paclitaxel measured	391 μ g
Percentage of paclitaxel recovered	80%

Example 8: Release kinetics of paclitaxel from polyurethane-based stent coating.

Slotted tube stainless steel stents are coated with polyurethane by spraying a 1 wt% solution of CHRONOFLEX® polyurethane (made by CT Biomaterials) in tetrahydrofuran directly onto the stent surface. The coated stents are dried in a vacuum oven for three hours at 70°C.

Each polyurethane coated stent is placed in a vial, which is filled to maximum volume (1.5 ml) with a solution of paclitaxel in ethanol, and sealed. The stent is stored in the vial for three days at room temperature. The stent is then removed from the vial and dried for one hour at 65°C.

The above procedure is conducted using solutions of varying concentrations. Each stent is analyzed for paclitaxel content by extraction in dichloromethane solvent. The results are presented in Table IV below. Samples 1 and 2 were obtained using a paclitaxel concentration of 10 mg/ml, samples 3 and 4 using a 20 mg/ml solution and sample 5 and 6 using a 30 mg/ml solution.

Table IV. Paclitaxel content.

Sample #	Paclitaxel conc. (mg/ml)	Paclitaxel content (μ g)	Coating Wt. (μ g)	μ g Paclitaxel per μ g coating
1	10	44.8	796	0.06
2	10	88.2	859	0.10
3	20	151.2	718	0.21
4	20	127.6	702	0.18
5	30	157.1	736	0.21
6	30	144.3	629	0.23

These results suggest that paclitaxel loading is relatively independent of paclitaxel concentration above 20 mg/ml, assuming equilibrium is attained in the three-day period. Nevertheless, the 30 mg/ml paclitaxel concentration is chosen for release studies as it produces the maximum paclitaxel loading (21-23%), while still being sufficiently below the saturation concentration for paclitaxel in ethanol (39 mg/ml).

Seven polyurethane coated stents are loaded using a 30 mg/ml paclitaxel solution, removed and dried as set forth above. Paclitaxel from four of the stents is extracted in dichloromethane solvent. The results of this extraction are presented in Table V below:

Table V. Paclitaxel content.

Sample #	Paclitaxel conc. (mg/ml)	Paclitaxel content (μ g)	Coating Wt. (μ g)	μ g Paclitaxel per μ g coating
1	30	111.7	676	0.17
2	30	50	627	0.08
3	30	45.3	612	0.07
4	30	37.4	602	0.06

The remaining three stents are immersed in a solution of phosphate buffered saline solution having pH 7.4 at 37°C. Cumulative release as a function of time is presented in Fig. 8.

Example 9: Release kinetics of paclitaxel from polyurethane-based balloon catheter coating.

Nylon balloons are coated with polyurethane by dipping into a 9 wt% solution of CHRONOFLEX® polyurethane in dimethylacetamide. The balloons are dried in a vacuum oven overnight at 50°C.

Each polyurethane coated balloon is loaded with paclitaxel either by dipping the coated balloon into a paclitaxel and ethanol solution or by dripping a known volume of a paclitaxel and ethanol solution onto the balloon surface.

In the first instance, a stock saturated solution

of paclitaxel in ethanol is prepared. Then the polyurethane-coated balloon is inflated and submerged in the paclitaxel stock solution in a tube. The tube and balloon are well-sealed to prevent solvent evaporation.

5 After remaining in the tube overnight, the ethanol is evaporated from the balloon over a suitable time period, such as about fifteen minutes. Five "dip-coated" balloons are prepared in this fashion.

In the second instance, a stock solution of
10 paclitaxel having a concentration of 10 mg/ml prepared. Twenty ml of this paclitaxel stock solution are then pipetted onto an inflated polyurethane-coated balloon, providing a total mass of 200 mg of paclitaxel per balloon. Afterwards, ethanol is evaporated from the balloon over a
15 suitable time period, such as about fifteen minutes. Five "drip-coated" balloons are prepared in this fashion.

Two drip-loaded balloons and two dip-loaded balloons are taken and the paclitaxel extracted in dichloromethane to determine total paclitaxel content. The
20 paclitaxel content of the dip-coated balloons is found to be 1093 +/- 439 μ g, while the drip-coated balloons are found to have 215 +/- 11 μ g paclitaxel.

For comparison, nylon balloons are coated with

paclitaxel/polyurethane by dipping the balloons into a dispersion of 14.5 wt% BAHYDROL® polyurethane (made by Bayer) and 2.6 wt% paclitaxel in a mixture of 73.6 vol% N-methylpyrrolidinone and 26.4 vol% water. Balloons are dried in a vacuum oven overnight at 50°C. The dried coatings contain 15% paclitaxel by weight. Nine balloons are formed. Seven balloons are tested for paclitaxel loading yielding an average of 196 +/- 44 µg paclitaxel after extraction in dichloromethane.

The remaining three drip-loaded balloons from above, the remaining three dip-loaded balloons from above, and the remaining two balloons with the 15% paclitaxel formulated coating are placed in a solution of phosphate buffered saline solution having pH 7.4 at 37°C, and cumulative paclitaxel release is measured as a function of time. The results of this study are presented in Fig. 9.

Example 10: Preparation of a stent coated with a polylactic acid/polycaprolactone (PLA/PCL) copolymer/paclitaxel matrix.

PLA/PCL copolymer obtained from Birmingham Polymers, Inc., Birmingham, Alabama, was dissolved in chloroform. Paclitaxel obtained from Hauser, Inc. was then dissolved in the chloroform to form a solution having a

70/30 weight ratio of copolymer/paclitaxel. The solution was then sprayed onto the surface of a 9 mm long balloon-expandable stainless steel NIR® stent obtained from Medinol, Inc., Tel Aviv, Israel. Substantially all exposed surfaces of the stent were covered with the solution. The stent was then dried in a vacuum oven at 50°C for approximately 2 hr. and a matrix of PLA/PCL copolymer having 200 µg of paclitaxel incorporated therein was thus formed as a coating on the stent. The paclitaxel component of the matrix comprised approximately 30% by weight of the matrix.

Example 11: In-vitro delivery of paclitaxel to porcine coronary arteries.

A stent prepared as set forth in Example 10 was inserted via a balloon catheter and expanded into contact with a porcine coronary artery. In vitro, the stent delivered 2-3 µg/day of paclitaxel over a period of 28 days. In comparison to the same stent having no coating, after 28 days, a 50% reduction in the occurrence of neointimal hyperplasia was observed.

Example 12: In-vitro delivery of paclitaxel to rabbit iliac.

A stent prepared as set forth in Example 10 was

inserted via a balloon catheter and expanded into contact with a rabbit iliac. In vitro, the stent delivered 2-3 $\mu\text{g/day}$ of paclitaxel over a period of 28 days. In comparison to the same stent having no coating, after 28 days, a 70% reduction in the occurrence of neointimal hyperplasia was observed.

Example 13: In-vitro delivery of paclitaxel to rabbit iliac.

A stent prepared as set forth in Example 10 was inserted via a balloon catheter and expanded into contact with a rabbit iliac. In vitro, the stent delivered 2-3 $\mu\text{g/day}$ of paclitaxel over a period of 56 days. In comparison to the same stent having no coating, after 56 days, a 60% reduction in the occurrence of neointimal hyperplasia was observed.

Comparative Example 14: Coil Stents with Biocompatible Polymeric Material/TAXOL® Coating.

The results presented in Table VI below were obtained by Leon et al., "TAXOL®-Coated Coronary Stents: Potential to Reduce Proliferation," European Society of Cardiology, Vienna, Austria 1998. GR-II® coil stents, available from Cook Inc., Bloomington, IN, were coated with

a biocompatible polymeric coating incorporating 175-200 μg of TAXOL® and exhibiting in vitro release kinetics of 0.75 $\mu\text{g/day}$ for the first 30 days. The stents were placed in porcine coronary arteries and the effect on neointima formation compared to that seen with control stents was analyzed. The results are shown in Table VI below:

Table VI: TAXOL®-Coated Stents versus Control

	Control (N=10)	TAXOL®-coated Stent (N=9)
Reference Vessel Diameter (mm)	2.9 \pm 0.3	3.0 \pm 0.2
Stent/Artery	1.1 \pm 0.1	1.1 \pm 0.1
Diameter Stenosis (%)	51 \pm 27	27 \pm 27*
Neointima Area (μm)	669 \pm 357	403 \pm 197*

*p<0.05 versus control

In contrast to the results obtained in Example 11 above using the NIR® non-coiled stent in a porcine coronary artery (neointimal hyperplasia reduction of 50%), the results obtained with a coil stent and paclitaxel (placed in a porcine coronary artery) show a neointimal hyperplasia reduction of only 40% calculated as follows: $[(669 - 403)/669] \times 100 = 40\%$.

Comparative Example 15: Comparison of Low-dose and High Dose TAXOL®-coated Stents versus control

The results of another study by Leon et al., "TAXOL®-Coated Coronary Stents: Potential to Reduce Proliferation," European Society of Cardiology, Vienna, Austria 1998 on the effect of coated coil stents on neointima formation using 2 doses of "fast-release" TAXOL® are shown in Table VII below: The results for both "low-dose" and "high-dose" TAXOL®-coated stents are shown in Table VII below:

Table VII: Low-Dose and High Dose TAXOL®-Coated Stents versus Control

	Control (N=12)	Low-Dose TAXOL® (N=10)	High-Dose TAXOL® (N=11)
Reference Vessel Diameter (mm)	2.8 ±0.2	2.8 ±0.7	3.0 ±0.3
Stent/Artery	1.16 ±0.09	1.15 ±0.07	1.14 ±0.05
Diameter Stenosis (%)	34.8 ±15.6	19.3 ±9.45*	15.1 ±6.61*†
Neointima Area (μm)	1.52 ±0.78	1.07 ±0.53	0.93 ±0.5*†

*p<0.05 versus control

†p=not significant versus low-dose TAXOL®

In contrast to the results obtained in Examples 11-13 above using the NIR® non-coiled stent (neointimal hyperplasia reduction of from 50-70%), the above results

obtained with a coated coil stent show a neointimal hyperplasia reduction of only 30% and 39%, respectively, calculated as follows: $[(1.52-1.07)/1.52] \times 100 = 30\%$ (low-dose TAXOL®) and $[(1.52-0.93)/1.52] \times 100 = 39\%$ (high-dose TAXOL®).

Example 16: Preparation of a vena cava filter coated with a polylactic acid/polycaprolactone (PLA/PCL) copolymer/paclitaxel matrix.

A filter for placement in the vena cava for capturing blood clots is coated with a PLA/PCL copolymer/paclitaxel matrix in the manner substantially as set forth in Example 10. The filter is sized and constructed to be compressed and passed through the vasculature of a patient to be anchored against an inner wall surface of a blood vessel for capturing blood clots in a blood stream passing therethrough. The filter is described in International Application No. WO 96/17634.

Example 17: Preparation of a vena cava filter coated with a polylactic acid/polycaprolactone (PLA/PCL) copolymer/paclitaxel matrix.

A filter for placement in the vena cava for capturing blood clots is coated with a PLA/PCL copolymer/paclitaxel matrix in the manner substantially as

set forth in Example 10. The filter is also adapted for placement in a blood vessel for capturing blood clots in a blood stream passing therethrough. This filter is provided with struts that minimize the risk of vessel damage if the vessel is compressed asymmetrically. The filter is described in International Application No. WO 96/12448.

Example 18: Preparation of a vascular graft coated with a polylactic acid/polycaprolactone (PLA/PCL) copolymer/paclitaxel matrix.

A woven synthetic vascular graft for replacement of a segment a blood vessel is coated with a PLA/PCL copolymer/paclitaxel matrix in a manner substantially as set forth in Example 10. The vascular graft is ravel-resistant due to inclusion of a fusible component and self-supporting due to inclusion of a stiffening component. The vascular graft is described in U.S. Patent No. 5,509,931.

It is to be appreciated that the parameters described in the above examples are merely illustrative and that the present invention is not so limited. For example, in each of the examples provided, any suitable polymer may be used for the polymer coating, any suitable drying time periods and temperatures may be used, any suitable organic solvent may be used, any suitable method for applying the

polymer coatings to the medical devices may be used, any suitable method for applying the drugs to the polymer coatings may be used, any suitable water-insoluble analogue of the disclosed drugs may be used, and any suitable drug loading concentrations may be used.

The present invention provides a previously unknown method and medical device for the localized delivery of substantially water-insoluble drugs. The present invention provides, in one embodiment, a paclitaxel/polymer coated stent which has an extended release rate of from about 0.2 to about 7 μ g per day, preferably in the range of from about 0.5 to about 5 μ g per day over an extended period of at least about 28 days. In a preferred embodiment of the invention, there is provided a polymer/paclitaxel coated non-coiled stent which has an extended release rate of paclitaxel and which reduces neointima formation in injured blood vessels and other body lumens into which it is placed. The extended release rate is effective to prevent, decrease, eliminate, or modify cellular proliferation associated with neointima formation and/or other proliferative disease or disorder.

Those with skill in the art may recognize various modifications to the embodiments of the invention described

and illustrated herein. Such modifications are meant to be covered by the spirit and scope of the appended claims.

We claim:

1. A method for preparing a medical device having a substantially water-insoluble drug coated thereon comprising the steps of:

providing a polymer;

providing a medical device adapted for insertion in a body;

coating at least a portion of the exterior surface of the medical device with the polymer to form a polymer coating; and

applying a drug solution to the polymer, said drug solution comprising at least one substantially water-insoluble drug dissolved in an organic solvent.

2. The method of claim 1, further comprising the step of drying said polymer coating such that substantially all of said solvent is evaporated.

3. The method of claim 1, wherein said polymer is selected from the group consisting of polycarboxylic acids, cellulosic polymers, gelatin, polyvinylpyrrolidone, maleic anhydride polymers, polyamides, polyvinyl alcohols, polyethylene oxides, glycosaminoglycans, polysaccharides, polyesters, polyacrylamides, polyethers, polyurethane dispersions, acrylic latex dispersions, polyalkylenes, proteins,

9 polypeptides, silicones, siloxanes, copolymers of
10 vinyl monomers, polyvinyl ethers, polylactic acid,
11 polycaprolactone, and mixtures and copolymers thereof.

1 4. The method of claim 3, wherein said polymer is
2 polyacrylic acid.

1 5. The method of claim 1, wherein said at least one
2 substantially insoluble drug is selected from the
3 group consisting of dexamethasone, molsidomine,
4 prednisolone, corticosterone, budesonide, estrogen,
5 sulfasalazine, mesalamine, paclitaxel, cisplatin,
6 vinblastine, vincristine, epothilones, endostatin,
7 angiostatin, lidocaine, bupivacaine and ropivacaine.

1 6. The method of claim 1, wherein said organic solvent is
2 selected from the group consisting of ethanol,
3 isopropanol, chloroform, acetone, pentane, hexane,
4 methylene chloride, and mixtures thereof.

1 7. The method of claim 6, wherein said organic solvent
2 further comprises water.

1 8. The method of claim 1, wherein said step of applying
2 a drug solution to said polymer includes the step of
3 dipping said polymer into said drug solution.

1 9. The method of claim 1, wherein said drug solution is
2 applied to said polymer before said polymer is coated
3 onto said medical device.

1 10. The method of claim 1, wherein said drug solution is
2 applied to said polymer after said polymer is coated
3 onto said medical device.

1 11. The method of claim 1, wherein said medical device is
2 selected from catheters, guide wires, balloons,
3 stents, vascular grafts, covered stents, stent grafts,
4 filters, intraluminal paving systems, wire guides,
5 cannulae, artificial limbs and artificial joints.

1 12. The method of claim 11, wherein said medical device is
2 a catheter comprising a shaft and an expandable
3 portion mounted on said shaft, at least a portion of
4 the exterior surface of the expandable portion being
5 covered with said polymer coating.

1 13. The method of claim 1, further comprising positioning
2 said medical device at a desired location in a body
3 lumen.

1 14. The method of claim 13, wherein said medical device is
2 a catheter comprising a shaft and an expandable
3 portion mounted on said shaft, at least a portion of
4 the exterior surface of the expandable portion being
5 covered with said polymer coating.

1 15. The method of claim 14, further comprising the step of
2 expanding said expandable portion of said catheter.

1 16. The method of claim 15, wherein said catheter
2 comprises a sheath member which is extendable over

3 said expandable portion.

1 17. The method of claim 16, further comprising the steps
2 of:

3
4 extending said sheath over said expandable
5 portion prior to said positioning; and

6
7 exposing said expandable portion from said sheath
8 prior to said expanding.

1 18. The method of claim 1, wherein said step of coating
2 comprises the step of applying multiple layers of said
3 polymer to said medical device.

1 19. The method of claim 1, wherein said medical device is
2 a stent.

1 20. The method of claim 1, wherein said drug is
2 paclitaxel.

1 21. The method of claim 1, wherein said medical device is
2 a stent and said drug is paclitaxel.

1 22. The method of claim 21, wherein said stent is a
2 patterned stent.

1 23. The method of claim 22, wherein said polymer is a
2 copolymer of polylactic acid and polycaprolactone.

1 24. A medical device for delivering a substantially water-

insoluble drug at a desired location within a body,
comprising:

a medical device adapted for insertion in a body;
and

a polymer coating containing at least one
substantially water-insoluble drug provided on at
least a portion of said medical device, wherein
said substantially water-insoluble drug has a
water-solubility no greater than 1 part drug to
30 parts water.

25. The medical device of claim 24, wherein said drug has
a water solubility no greater than 1 part drug to
1,000 parts water.

26. The medical device of claim 24, wherein said medical
device is a catheter for delivering substantially
water-insoluble drugs to a desired location within a
body lumen, said catheter comprising:

a shaft;

an expandable portion mounted on said shaft; and

a polymer coating on at least a portion of said
expandable portion of said catheter, said polymer
coating being impregnated with at least one
substantially water-insoluble drug.

- 1 27. The medical device of claim 26, wherein said
2 expandable portion includes an inflatable balloon.
- 1 28. The medical device of claim 27, further comprising a
2 sheath member extendable over said expandable portion.
- 1 29. The medical device of claim 24, wherein said polymer
2 is selected from the group consisting of
3 polycarboxylic acids, cellulosic polymers, gelatin,
4 polyvinylpyrrolidone, maleic anhydride polymers,
5 polyamides, polyvinyl alcohols, polyethylene oxides,
6 glycosaminoglycans, polysaccharides, polyesters,
7 polyacrylamides, polyethers, polyurethane dispersions,
8 acrylic latex dispersions, polyalkylenes, proteins,
9 polypeptides, silicones, siloxanes, copolymers of
10 vinyl monomers, polyvinyl ethers, polylactic acid,
11 polycaprolactone, and mixtures and copolymers thereof.
- 1 30. The medical device of claim 29, wherein said polymer
2 is polyacrylic acid.
- 1 31. The medical device of claim 24, wherein said at least
2 one substantially water-insoluble drug is selected
3 from the group consisting of dexamethasone,
4 molsidomine, prednisolone, corticosterone, budesonide,
5 estrogen, sulfasalazine, mesalamine, paclitaxel,
6 cisplatin, vinblastine, vincristine, epothilones,
7 endostatin, angiostatin, lidocaine, bupivacaine and
8 ropivacaine.
- 1 32. The medical device of claim 27, wherein said

2 expandable portion includes a stent.

1 33. The medical device of claim 24, wherein said polymer
2 coating is layered.

1 34. The medical device of claim 24, wherein said polymer
2 is polyurethane.

1 35. The medical device of claim 24, wherein said medical
2 device is a stent.

1 36. The medical device of claim 24, wherein said drug is
2 paclitaxel.

1 37. The medical device of claim 24, wherein said medical
2 device is a stent and said drug is paclitaxel.

1 38. The medical device of claim 37, wherein said stent is
2 a patterned stent.

3

4 39. The medical device of claim 38, wherein said polymer
5 is a copolymer of polylactic acid and
6 polycaprolactone.

7

8 40. The medical device of claim 38 wherein the at least
9 one water-insoluble drug comprises a combination of
10 paclitaxel and an agent selected from the group
11 consisting of anticoagulants, antimitotics,
12 antithrombogenics, thrombolytics, anti-inflammatory
13 agents, antioxidants, growth factors, modulators of
14 vascular homeostasis, cytocidal agents, and cytostatic

15 agents.

1 41. The medical device of claim 37, wherein the paclitaxel
2 is released from said device over a time frame
3 effective to inhibit proliferative disease when said
4 stent is positioned at a site of injury to thereby
5 prevent or inhibit undesired cellular proliferation.

1 42. The medical device of claim 40, wherein the time
2 frame is at least about 7 days.

1 43. The medical device of claim 40, wherein the time frame
2 is at least about 28 days.

1 44. The medical device of claim 40, wherein the paclitaxel
2 is released at a rate in the range of from about 0.2
3 to about 7 μg paclitaxel per day.

1 45. The medical device of claim 40, wherein the paclitaxel
2 is released at a rate in the range of from about 0.5
3 to about 5 μg per day.
4

5 46. The medical device of claim 37, wherein the device
6 inhibits neointimal proliferation when placed at the
7 site of injury in a blood vessel.
8

1 47. A polymer containing at least one substantially water-
2 insoluble drug.

1 48. The polymer of claim 45, wherein said polymer is
2 selected from the group consisting of polycarboxylic

3 acids, cellulosic polymers, gelatin,
4 polyvinylpyrrolidone, maleic anhydride polymers,
5 polyamides, polyvinyl alcohols, polyethylene oxides,
6 glycosaminoglycans, polysaccharides and derivatives
7 thereof, polyesters, polyacrylamides, polyethers,
8 polyurethane dispersions, acrylic latex dispersions,
9 polyalkylenes, proteins, polypeptides, silicones,
10 siloxanes, copolymers of vinyl monomers, polyvinyl
11 ethers, polylactic acid, polycaprolactone, and
12 mixtures and copolymers thereof.

1 49. The polymer of claim 46, wherein said polymer is
2 polyacrylic acid.

1 50. The polymer of claim 45, wherein said at least one
2 substantially water-insoluble drug is selected from
3 the group consisting of dexamethasone, molsidomine,
4 prednisolone, corticosterone, budesonide, estrogen,
5 sulfasalazine, mesalamine, paclitaxel, cisplatin,
6 vinblastine, vincristine, epothilones, endostatin,
7 angiostatin, lidocaine, bupivacaine and ropivacaine.

1 51. The polymer of claim 45, wherein said polymer is
2 polyurethane.

1 52. The polymer of claim 40, wherein said polymer is a
2 copolymer of polylactic acid and polycaprolactone.

1 53. The polymer of claim 45, wherein said drug is
2 paclitaxel.

1 54. The polymer of claim 45, wherein said polymer is
2 polyurethane and said drug is paclitaxel.

1 55. The polymer of claim 45, wherein said polymer is a
2 copolymer of polylactic acid and polycaprolactone and
3 said drug is paclitaxel.
4

5 56. A method of preventing or inhibiting proliferative
6 disease at a site of blood vessel injury in a patient
7 comprising implanting a patterned stent comprising an
8 outer coating of polymer/paclitaxel at the site of
9 injury, wherein the paclitaxel is released from the
10 outer coating at a release rate and for a period of
11 time sufficient to inhibit or prevent cellular
12 proliferation at the site of injury.
13

14 57. The method of claim 56, wherein the paclitaxel is
15 released from the outer coating for a period of time
16 from about 7 to about 28 days.
17

18 58. The method of claim 56, wherein the paclitaxel is
19 released from the outer coating at a release rate of
20 from about 0.2 to about 7 $\mu\text{g/day}$.
21

22 59. The method of claim 56, wherein the paclitaxel is
23 released from the outer coating at a release rate and
24 for a period of time sufficient to inhibit or prevent
25 neointima formation at the site of injury.
26

27 60. The method of claim 56, wherein the proliferative
28 disease is restenosis.

- 29
- 30 61. The method of claim 56, wherein the stent comprises an
- 31 outer coating of a polylactic acid/polycaprolactone
- 32 copolymer and paclitaxel.
- 33
- 34 62. A method of preventing or inhibiting proliferative
- 35 disease in a patient comprising
- 36 implanting a patterned stent comprising an outer
- 37 coating of polymer/paclitaxel at a site of cellular
- 38 proliferation, wherein the paclitaxel is released
- 39 from the outer coating at a release rate and for a
- 40 period of time sufficient to inhibit or prevent
- 41 cellular proliferation at the site.
- 42
- 43 63. The method of claim 62, wherein the paclitaxel is
- 44 released from the outer coating for a period of time
- 45 from about 7 to about 28 days.
- 46
- 47 64. The method of claim 62, wherein the paclitaxel is
- 48 released from the outer coating at a release rate of
- 49 from about 0.2 to about 7 $\mu\text{g}/\text{day}$.
- 50
- 51 65. The method of claim 62, wherein the paclitaxel is
- 52 released from the outer coating at a release rate and
- 53 for a period of time sufficient to inhibit or prevent
- 54 neointima formation at the site.
- 55
- 56 66. The method of claim 62, wherein the proliferative
- 57 disease is restenosis.
- 58
- 59 67. The method of claim 62, wherein the stent comprises an

60 outer coating of a polylactic acid/polycaprolactone
61 copolymer and paclitaxel.

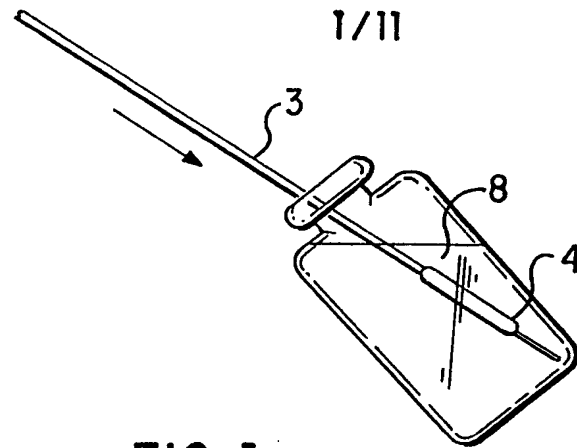


FIG. 1a

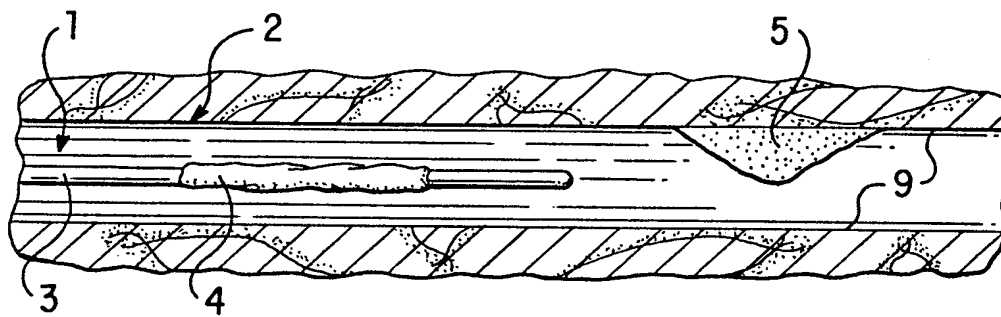


FIG. 1b

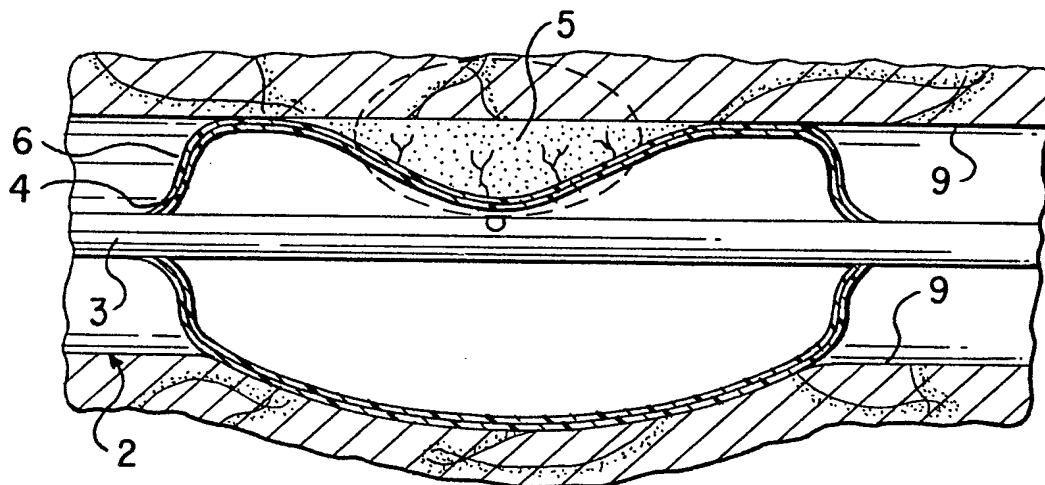


FIG. 1c

2/11

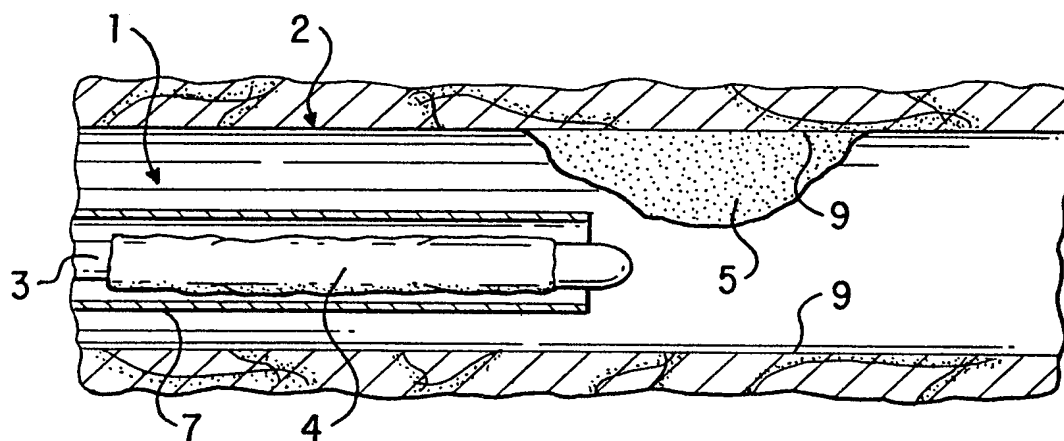


FIG. 2a

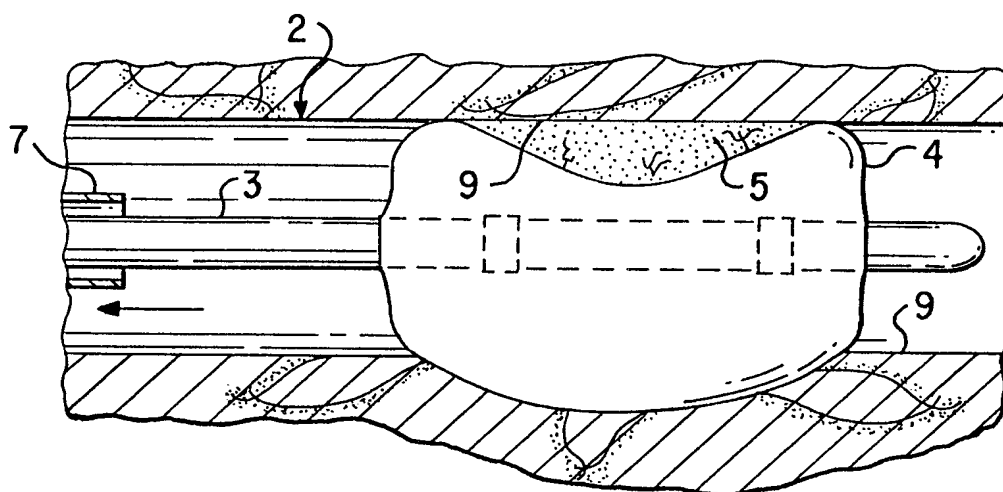


FIG. 2b

3/11

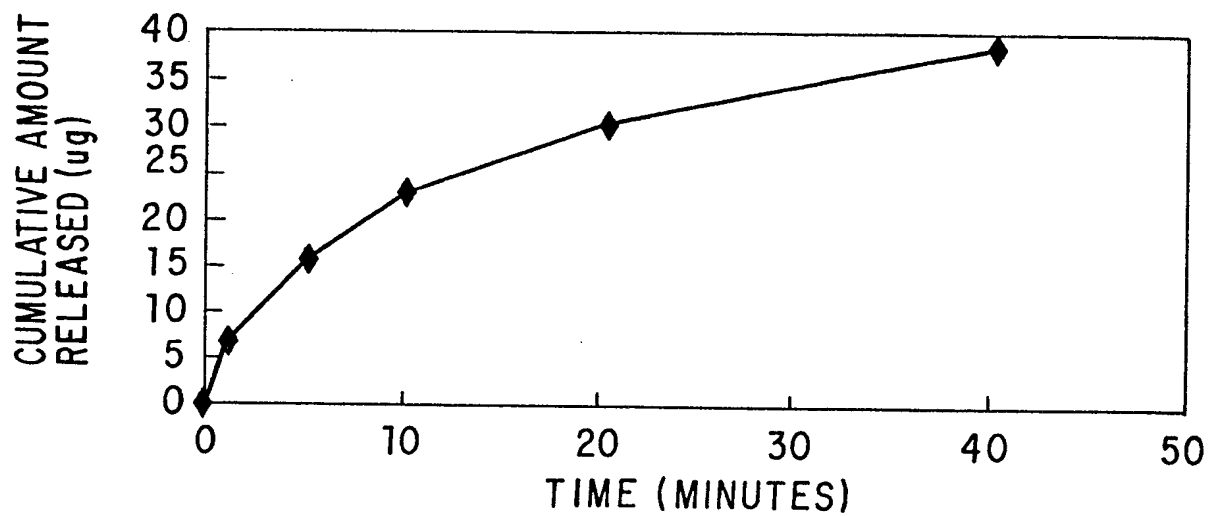


FIG. 3a

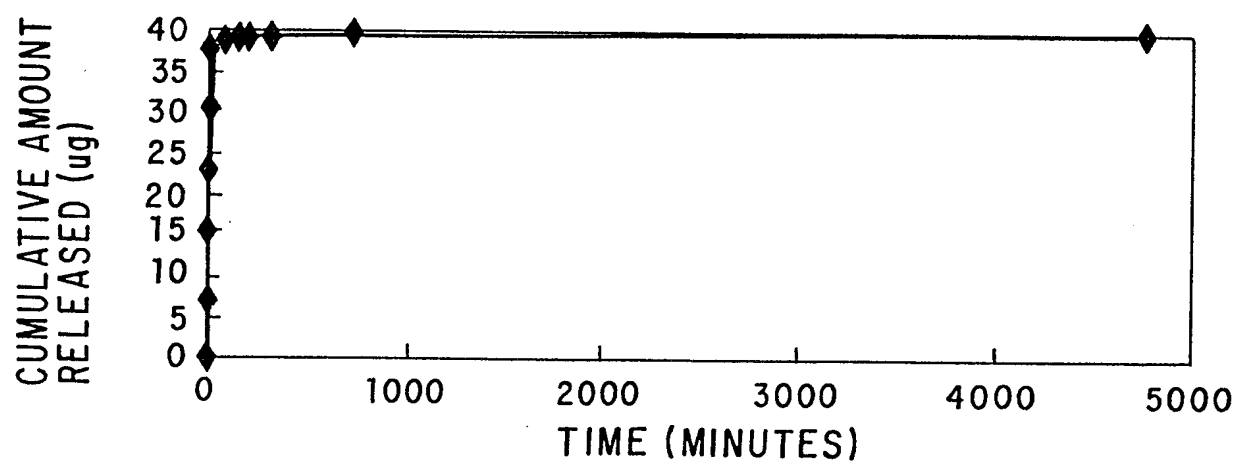


FIG. 3b

4/11

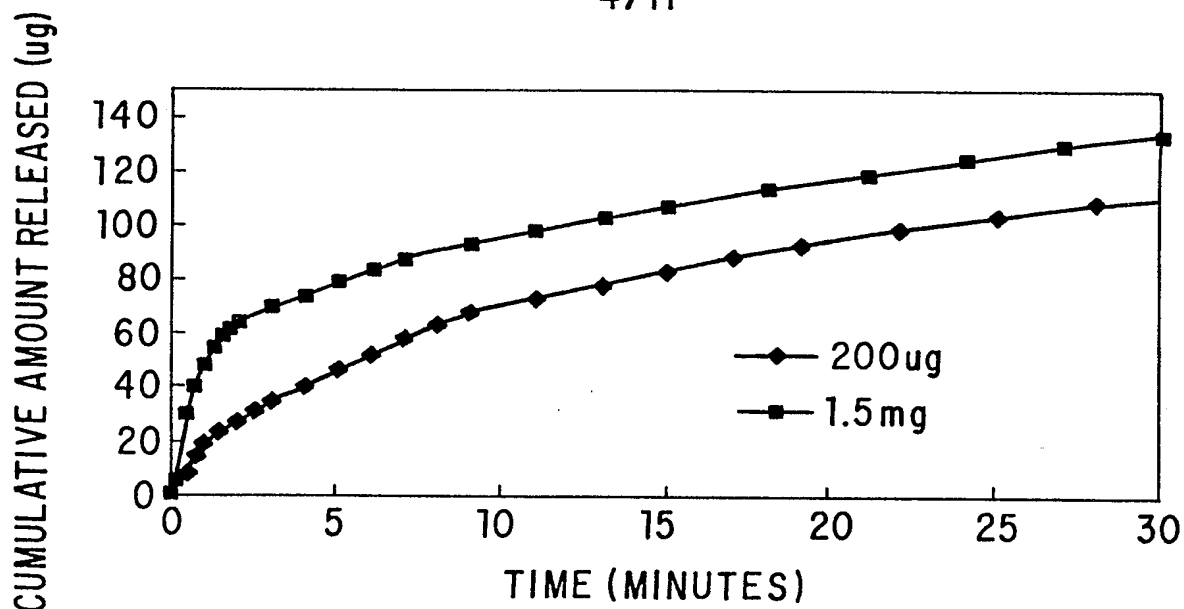


FIG. 4a

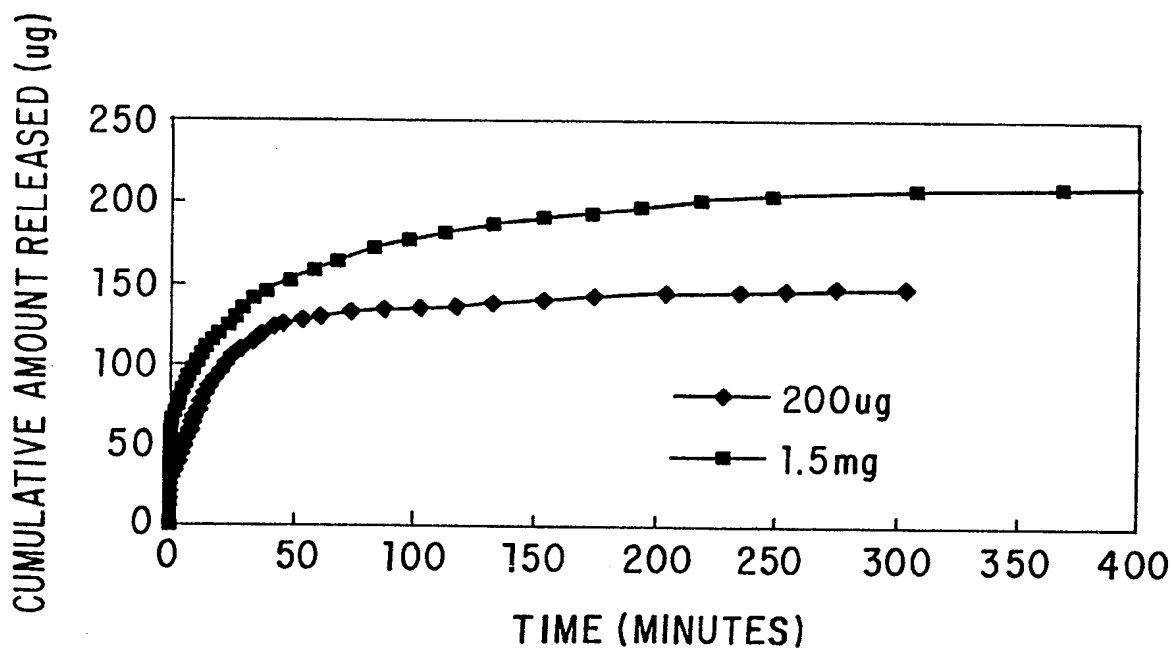


FIG. 4b

5/11

5/11

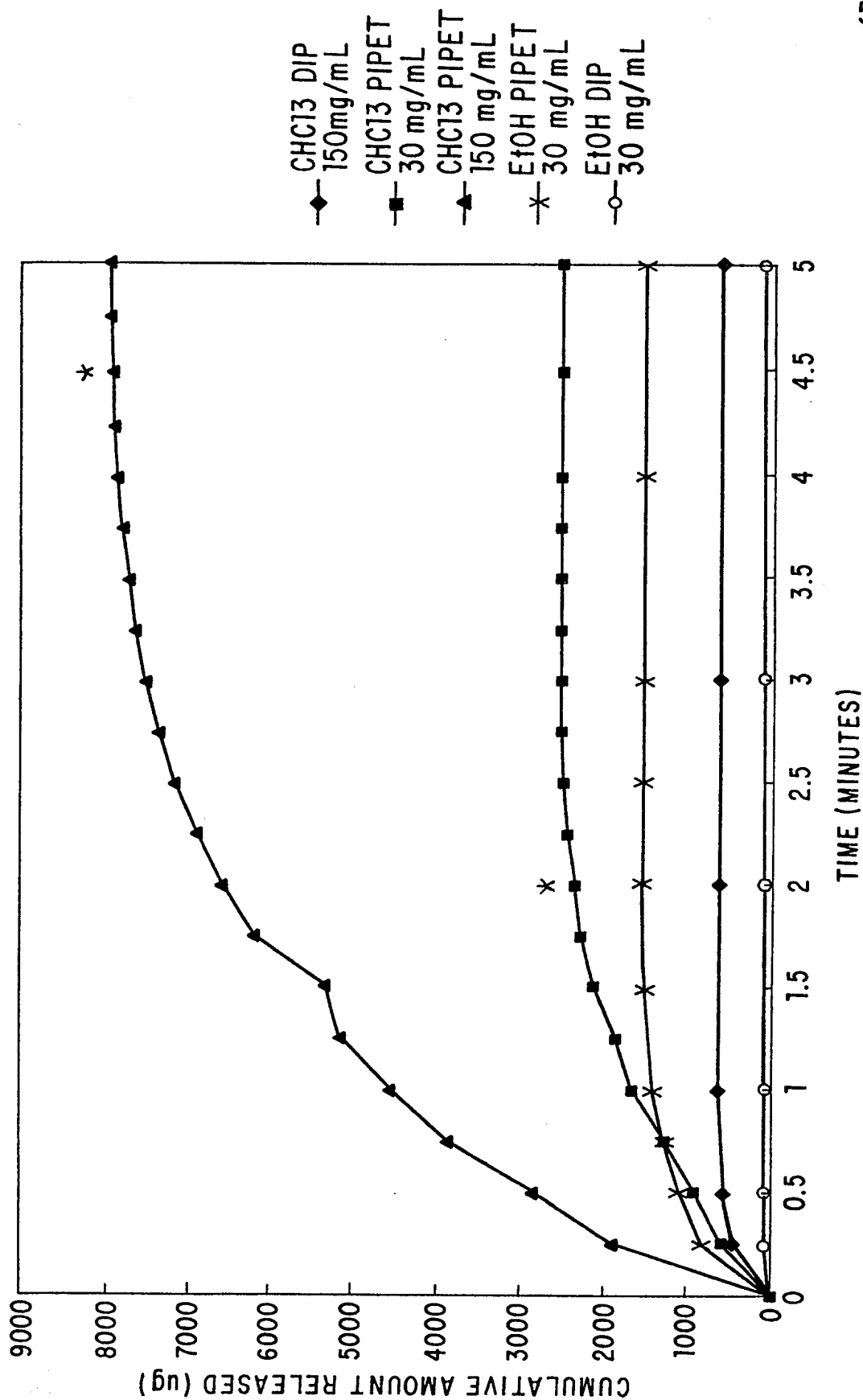


FIG. 5

6/11

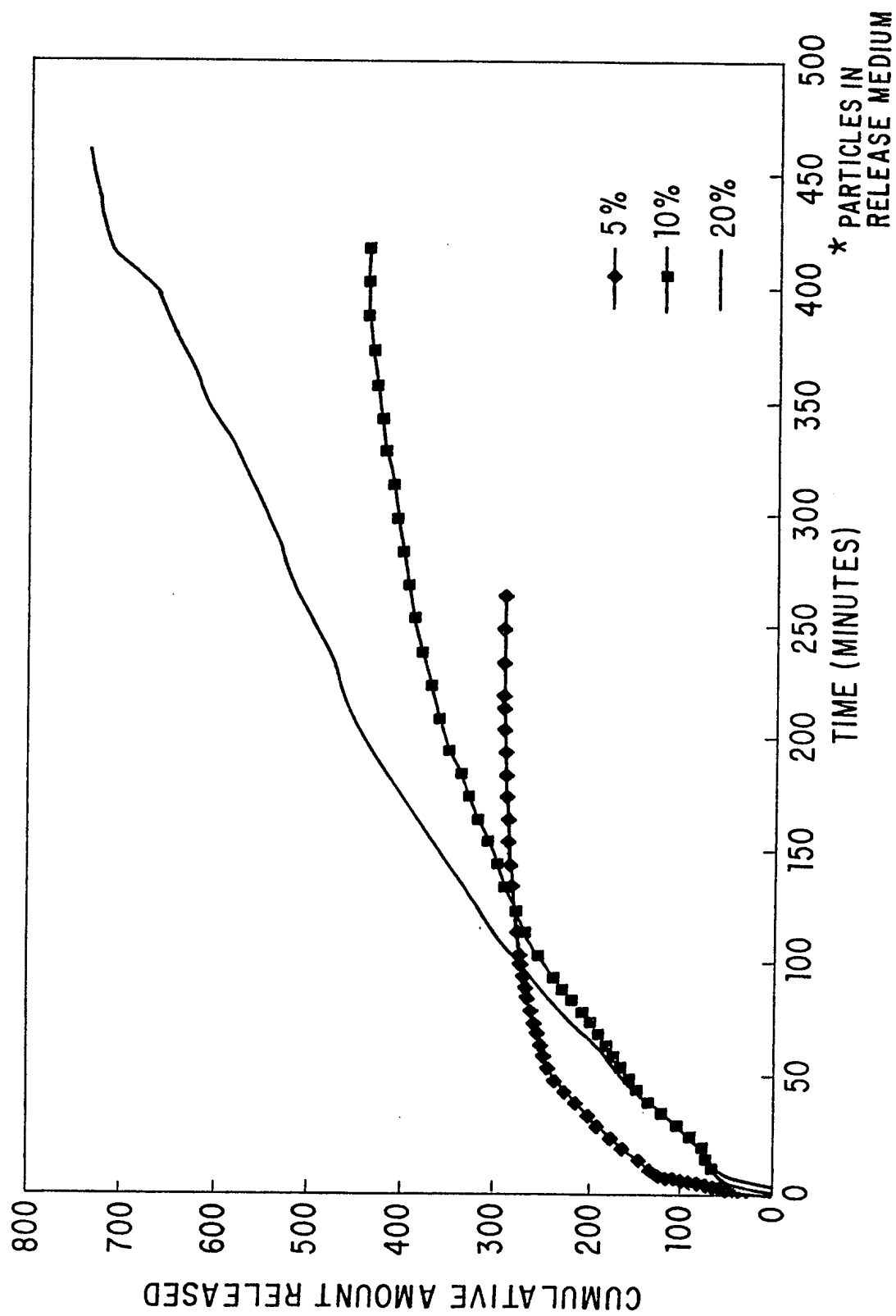


FIG. 6

7/11

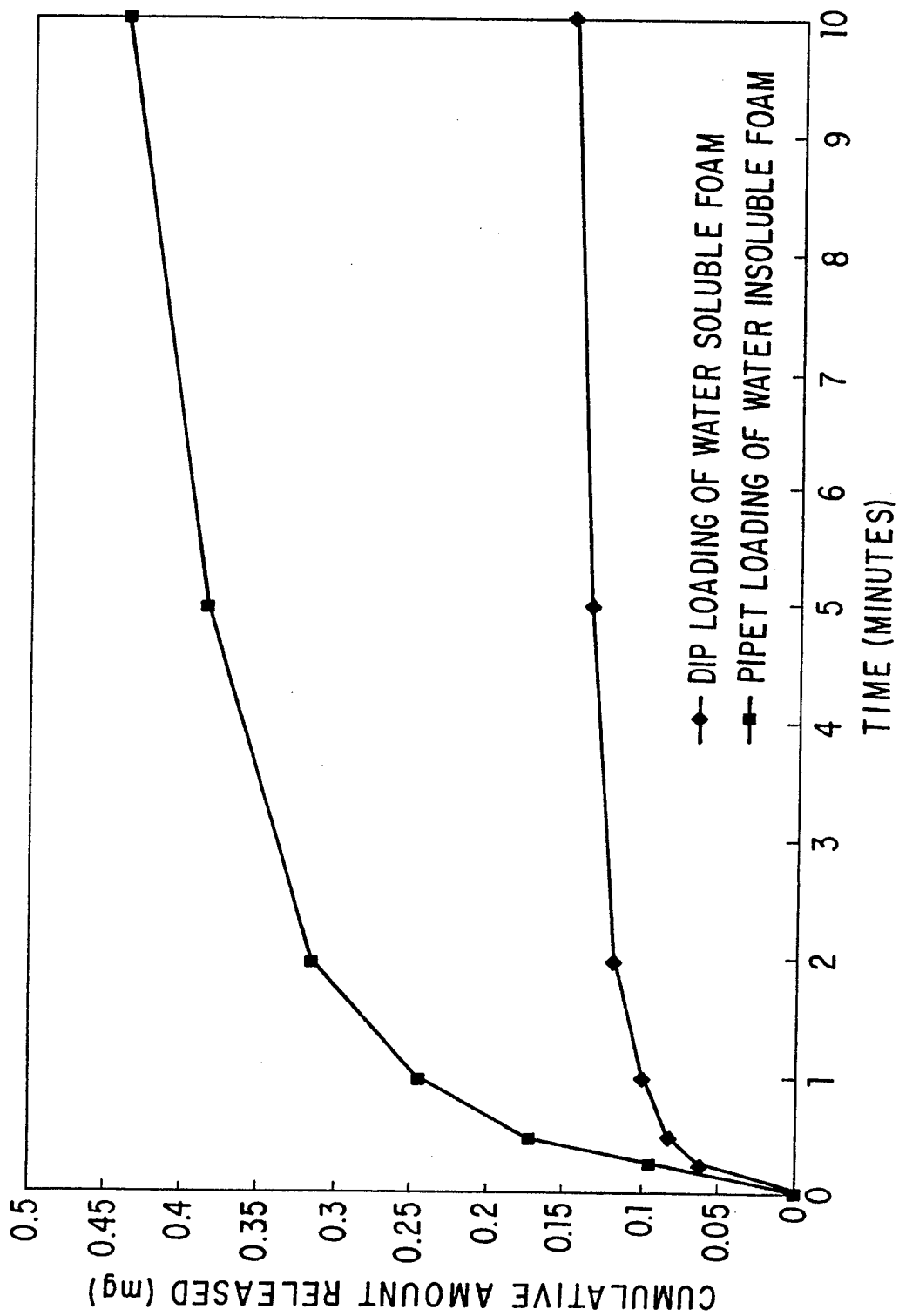


FIG. 7a

8/11

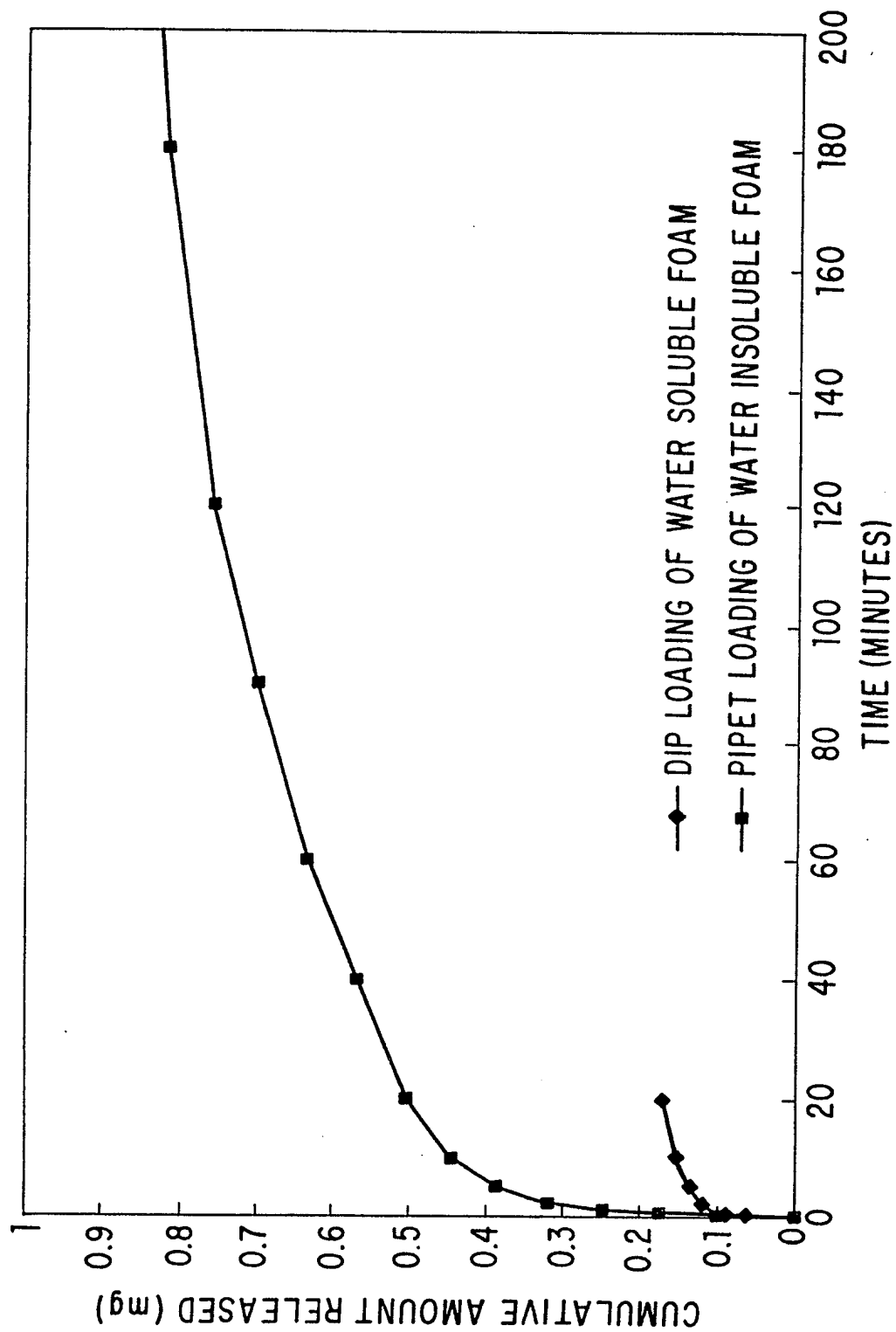


FIG. 7b

9/11

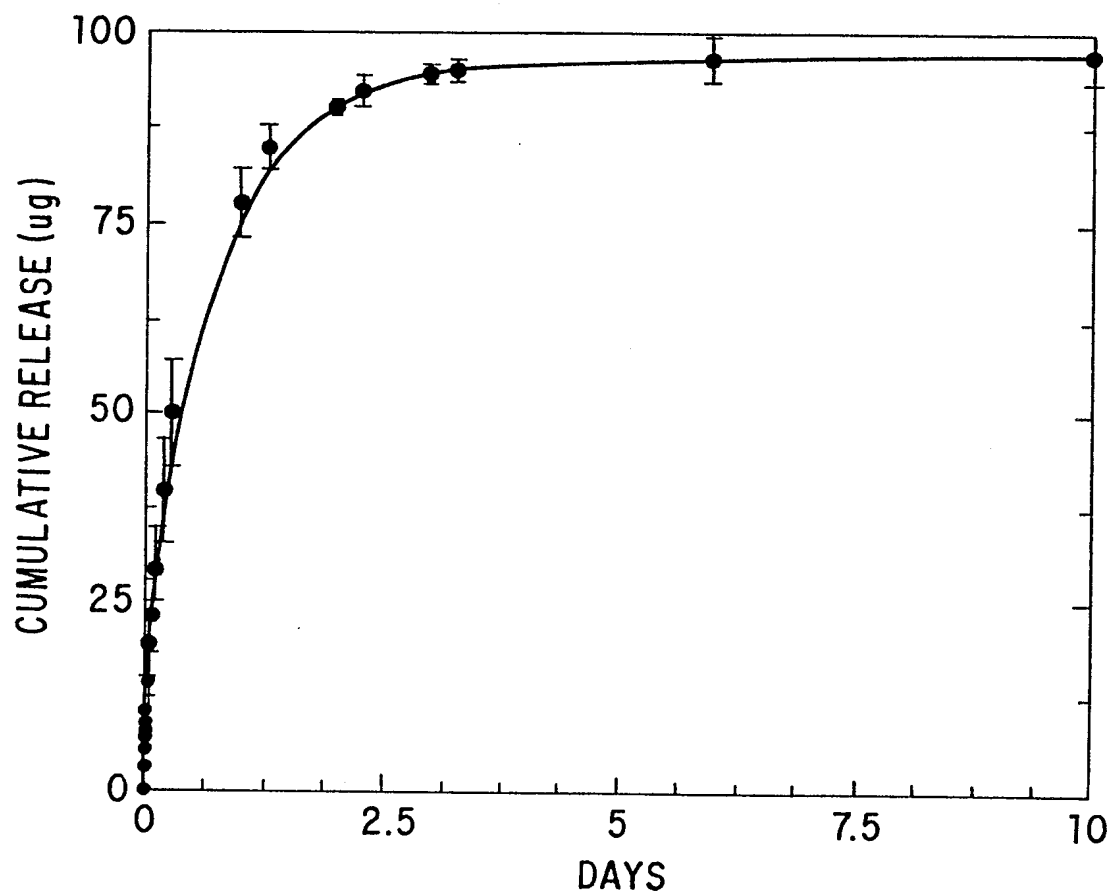


FIG. 8

10/11

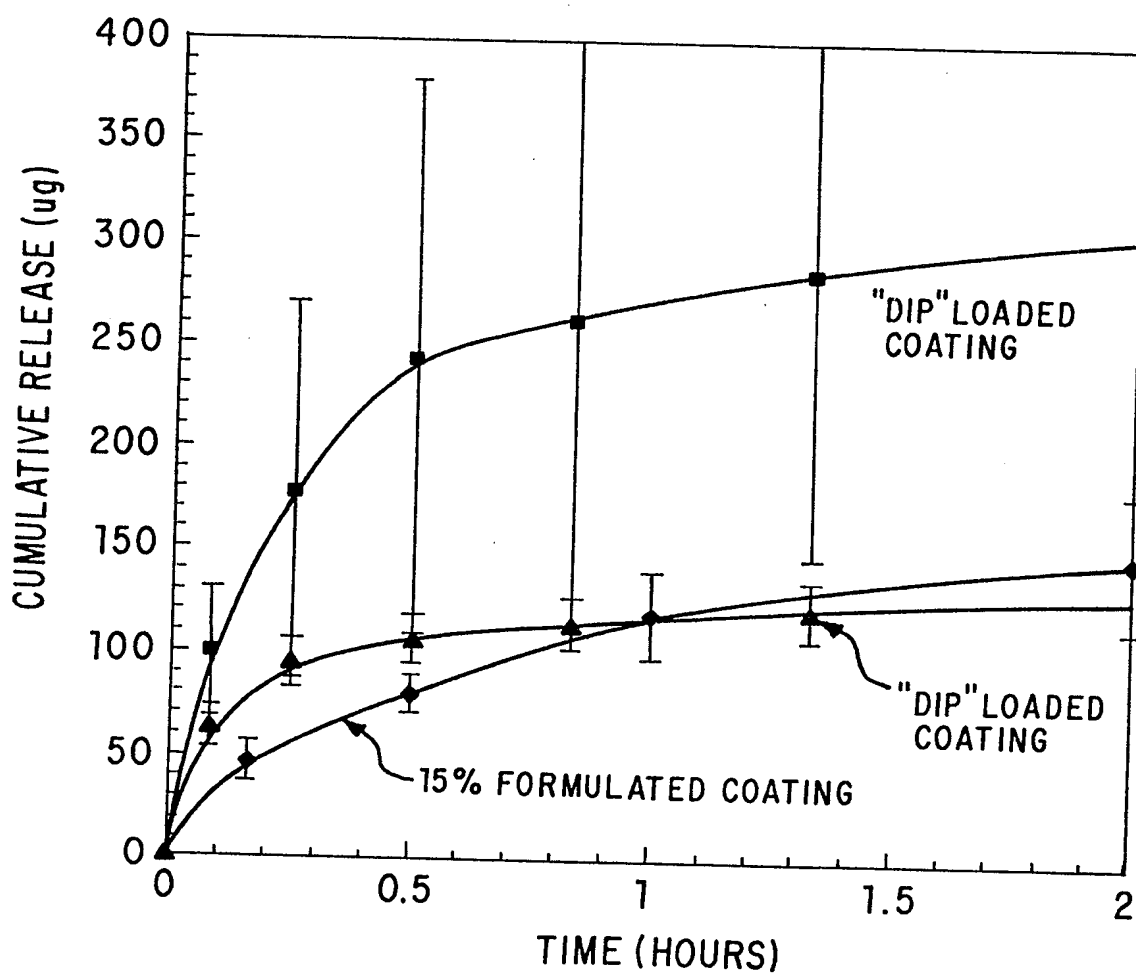


FIG. 9

11/11

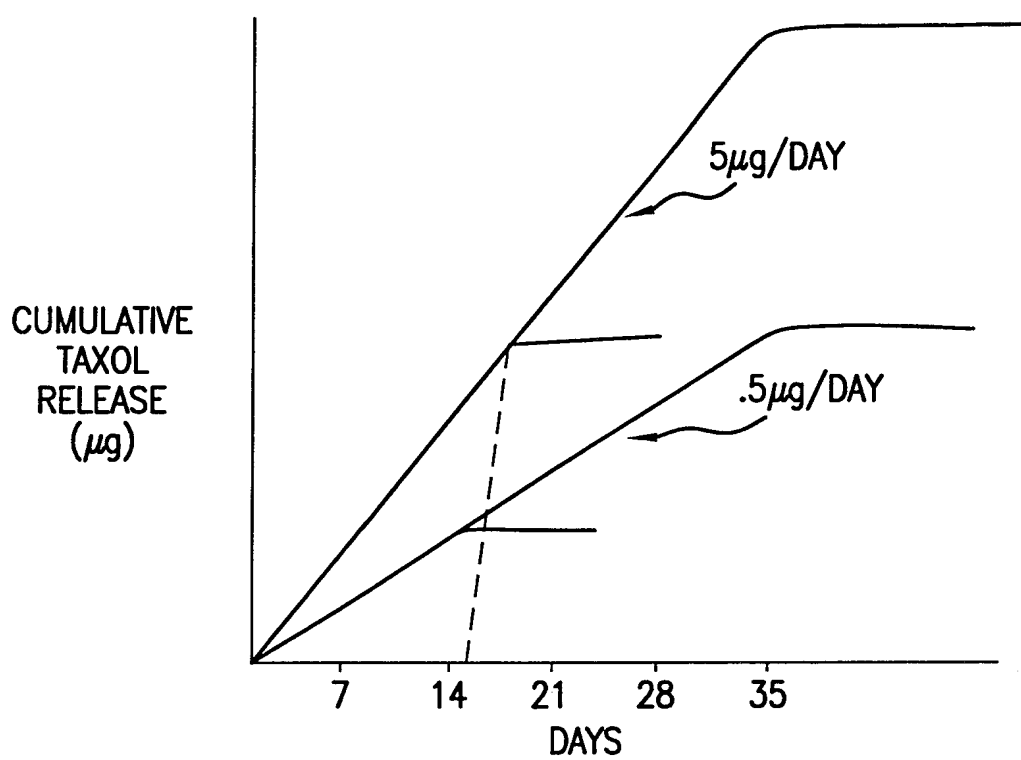


FIG.10

INTERNATIONAL SEARCH REPORT

International Application No

PCT/US 99/23654

A. CLASSIFICATION OF SUBJECT MATTER

IPC 7 A61L29/16 A61L27/54 A61L31/16 A61L29/08 A61L31/10

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

IPC 7 A61L

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	<p>WO 95 03036 A (ANGIOGENESIS TECH INC ; ARSENAULT A LARRY (CA); BURT HELEN M (CA);) 2 February 1995 (1995-02-02)</p> <p>page 4, line 17 -page 6, line 15 page 21, line 2 -page 22, line 12 claims 1-14</p> <p>---</p> <p>-/--</p>	<p>1-3, 5-17, 19-29, 31, 32, 35-48, 50, 52-67</p>

☒ Further documents are listed in the continuation of box C.

☒ Patent family members are listed in annex.

* Special categories of cited documents:

- "A" document defining the general state of the art which is not considered to be of particular relevance
- "E" earlier document but published on or after the international filing date
- "L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)
- "O" document referring to an oral disclosure, use, exhibition or other means
- "P" document published prior to the international filing date but later than the priority date claimed

- "T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
- "X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
- "Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.
- "&" document member of the same patent family

Date of the actual completion of the international search

7 February 2000

Date of mailing of the international search report

14/02/2000

Name and mailing address of the ISA

European Patent Office, P.B. 5818 Patentlaan 2
NL - 2280 HV Rijswijk
Tel. (+31-70) 340-2040, Tx. 31 651 epo nl,
Fax: (+31-70) 340-3016

Authorized officer

Menidjel, R

INTERNATIONAL SEARCH REPORT

International Application No

PCT/US 99/23654

C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT

Category	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No
X	<p>US 5 674 192 A (BARRY JAMES J ET AL) 7 October 1997 (1997-10-07)</p> <p>column 1, line 50 -column 2, line 49 column 3, line 15 - line 55 figures 1,1B,1C</p> <p>---</p>	<p>1-17,19, 24-33, 35,37, 38,40, 41, 46-50, 56,60, 62,66</p>
X	<p>US 5 624 411 A (TUCH RONALD J) 29 April 1997 (1997-04-29)</p> <p>column 2, line 31 -column 3, line 27 column 5, line 15 - line 54 examples 1-7</p> <p>---</p>	<p>1-3, 5-19, 24-29, 31-35, 37,38, 40,41, 46-48, 50,51, 56,62,66</p>
X	<p>EP 0 623 354 A (MEDTRONIC INC) 9 November 1994 (1994-11-09)</p> <p>abstract page 2, line 40 -page 3, line 22 page 4, line 10 - line 47 table 1</p> <p>---</p>	<p>1-3, 5-19, 24-29, 31-35, 37,38, 40,41, 46-48, 50,51, 56,62,66</p>
P,X	<p>WO 99 08729 A (BOSTON SCIENT CORP) 25 February 1999 (1999-02-25)</p> <p>page 2, line 7 - line 29 page 4, line 16 -page 7, line 37 examples 1-9 figure 1C</p> <p>-----</p>	<p>1-22, 24-38, 40-51, 53-66</p>

INTERNATIONAL SEARCH REPORT

International application No.

PCT/US 99/23654

Box I Observations where certain claims were found unsearchable (Continuation of item 1 of first sheet)

This International Search Report has not been established in respect of certain claims under Article 17(2)(a) for the following reasons:

1. ☒ Claims Nos.: —
because they relate to subject matter not required to be searched by this Authority, namely:
Although claims 56-67 are directed to a method of treatment of the human/animal body, the search has been carried out and based on the alleged effects of the compound/composition.
2. ☐ Claims Nos.:
because they relate to parts of the International Application that do not comply with the prescribed requirements to such an extent that no meaningful International Search can be carried out, specifically:
3. ☐ Claims Nos.:
because they are dependent claims and are not drafted in accordance with the second and third sentences of Rule 6.4(a).

Box II Observations where unity of invention is lacking (Continuation of item 2 of first sheet)

This International Searching Authority found multiple inventions in this international application, as follows:

1. ☐ As all required additional search fees were timely paid by the applicant, this International Search Report covers all searchable claims.
2. ☐ As all searchable claims could be searched without effort justifying an additional fee, this Authority did not invite payment of any additional fee.
3. ☐ As only some of the required additional search fees were timely paid by the applicant, this International Search Report covers only those claims for which fees were paid, specifically claims Nos.:
4. ☐ No required additional search fees were timely paid by the applicant. Consequently, this International Search Report is restricted to the invention first mentioned in the claims; it is covered by claims Nos.:

Remark on Protest

- ☐ The additional search fees were accompanied by the applicant's protest.
- ☐ No protest accompanied the payment of additional search fees.

FURTHER INFORMATION CONTINUED FROM PCT/ISA/ 210

Continuation of Box I.1

Although claims 56-67 are directed to a method of treatment of the human/animal body, the search has been carried out and based on the alleged effects of the compound/composition.

Continuation of Box I.1

Rule 39.1(iv) PCT - Method for treatment of the human or animal body by surgery

FURTHER INFORMATION CONTINUED FROM PCT/ISA/ 210

Continuation of Box 1.1

Rule 39.1(iv) PCT - Method for treatment of the human or animal body
by surgery

INTERNATIONAL SEARCH REPORT

Information on patent family members

International Application No

PCT/US 99/23654

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
WO 9503036 A	02-02-1995	AT 154757 T	15-07-1997
		AU 6991198 A	16-07-1998
		AU 693797 B	09-07-1998
		AU 7119294 A	20-02-1995
		CA 2167268 A	02-02-1995
		CN 1130866 A	11-09-1996
		DE 69403966 D	31-07-1997
		DE 69403966 T	05-02-1998
		DK 706376 T	13-10-1997
		EP 0706376 A	17-04-1996
		EP 0797988 A	01-10-1997
		ES 2106553 T	01-11-1997
		GR 3024833 T	30-01-1998
		JP 9503488 T	08-04-1997
		NO 960226 A	18-03-1996
		NZ 268326 A	19-12-1997
		US 5886026 A	23-03-1999
		US 5716981 A	10-02-1998
		US 5994341 A	30-11-1999
US 5674192 A	07-10-1997	US 5304121 A	19-04-1994
		CA 2166101 A	02-02-1995
		EP 0708671 A	01-05-1996
		JP 9500561 T	21-01-1997
		WO 9503083 A	02-02-1995
		US 5954706 A	21-09-1999
		US 5843089 A	01-12-1998
		CA 2098984 A	29-06-1992
		DE 69131486 D	02-09-1999
		EP 0565604 A	20-10-1993
		EP 0920843 A	09-06-1999
		JP 6503984 T	12-05-1994
		WO 9211896 A	23-07-1992
		WO 9211895 A	23-07-1994
US 5624411 A	29-04-1997	US 5464650 A	07-11-1995
		EP 0623354 A	09-11-1994
		JP 8033718 A	06-02-1996
		US 5837008 A	17-11-1998
		US 5679400 A	21-10-1997
		US 5776184 A	07-07-1998
		US 5824048 A	20-10-1998
EP 0623354 A	09-11-1994	US 5464650 A	07-11-1995
		JP 8033718 A	06-02-1996
		US 5837008 A	17-11-1998
		US 5679400 A	21-10-1997
		US 5624411 A	29-04-1997
		US 5776184 A	07-07-1998
		US 5824048 A	20-10-1998
WO 9908729 A	25-02-1999	AU 8782098 A	08-03-1999